



DC and AC Electrokinetics

- Dielectrophoresis
- Electro-osmosis

References:

- Pohl, H.A., *Dielectrophoresis: The Behavior of Neutral Matter in Nonuniform Electric Fields* (Cambridge University Press, Cambridge, 1978).
- T. B. Jones, *Electromechanics of particles* (Cambridge University Press, Cambridge, 1995).
- Kirby, BJ, "Micro- and Nanoscale Fluid Mechanics: Transport in Microfluidic Devices," Cambridge University Press, 2010.



Dielectrophoresis (DC Field)

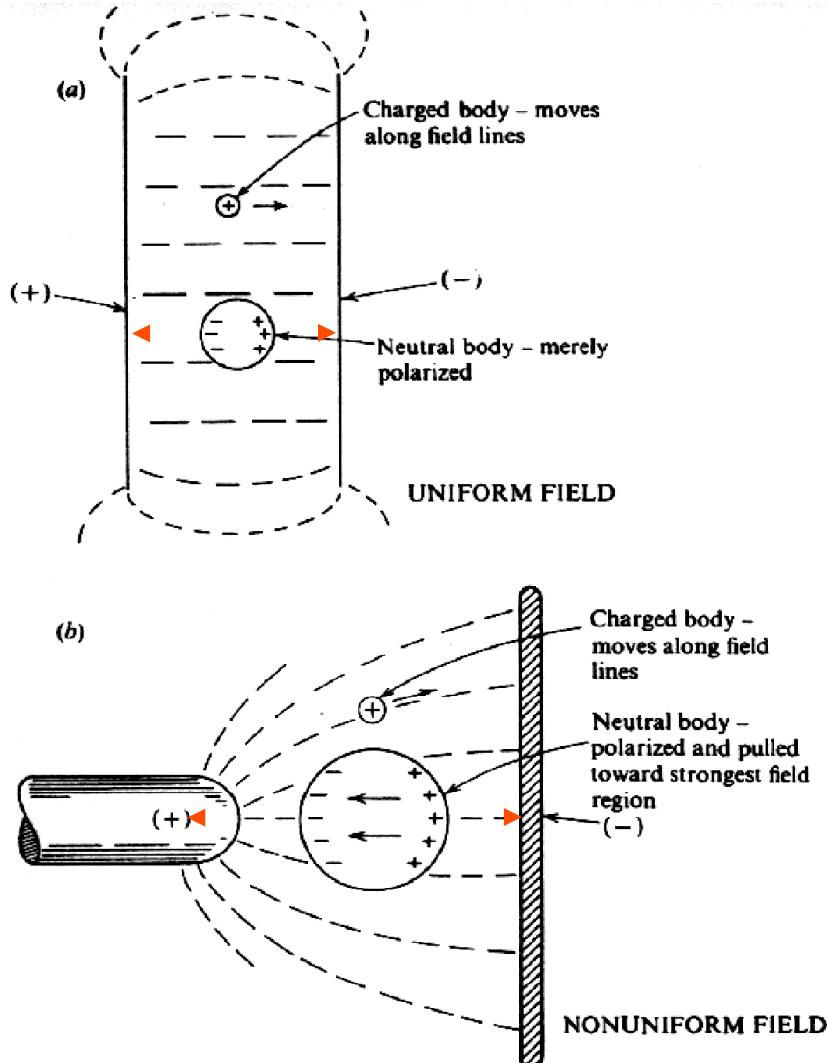


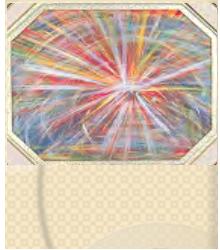
Fig. 2.1. Comparison of behaviors of neutral and charged bodies in (a) a uniform electric field; (b) a nonuniform electric field.

Uniform DC field:
Dielectric (neutral) object stays still

Non-uniform DC field:
Dielectric object moves

- towards **high-field gradient region (+DEP)**
- towards **low-field gradient region (-DEP)**

Pohl (1978)



Dielectrophoresis (AC Field)

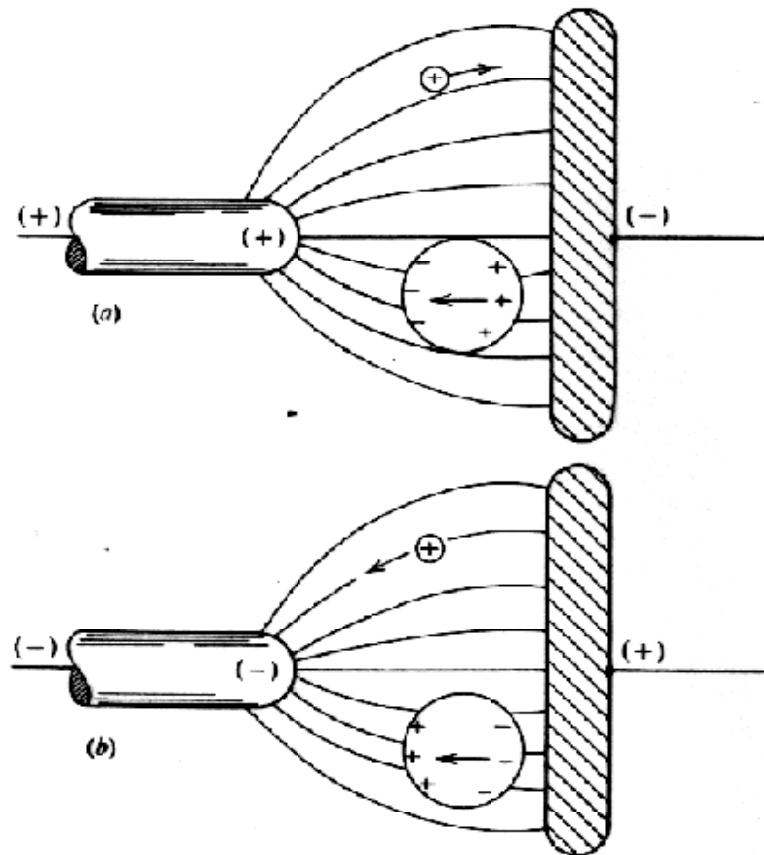


Fig. 2.2. Comparison of behaviors of neutral and charged bodies in an alternating nonuniform electric field.

In Non-uniform AC Field:

Charged body displays
no net displacement

Neutral body (dielectric) object
moves

- towards **high-field gradient region**
(+DEP) → trapping!
- towards **low-field gradient region**
(-DEP) → repelling!



Dielectrophoresis (DEP)

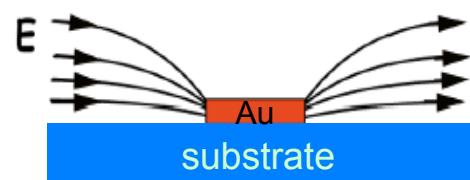
The classical DEP theory states that the dielectrophoretic force arises from the interaction of the induced dipole of a polarizable object and an external **non-uniform** electric field (Pohl 1978).

DEP is a technique which can be used to separate cells or molecules based on the difference in their polarizability.

Potential energy of a dielectric object in an electric field:

$$U = -\mathbf{p} \cdot \mathbf{E} = -\alpha V \mathbf{E}^2$$

a. Metallic trap



(Side view)

Dielectrophoretic force:

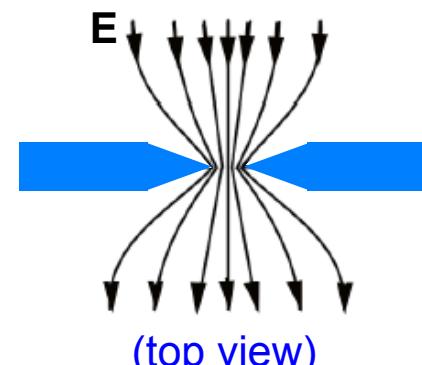
$$\mathbf{F} = -\nabla U \sim \mathbf{E}(d\mathbf{E}/dy)$$

$$F = 2\pi a^3 \epsilon_n \text{Re} \left(\frac{\epsilon_p^* - \epsilon_m^*}{\epsilon_p^* + 2\epsilon_m^*} \right) \nabla(E^2)$$

Clausius-Mossotti factor

Sphere of radius a ,
 $\epsilon_m = 80$ for water

b. Electrodeless trap (EDEP)





Application of DEP in Biology and ...

– Cells

- ❖ Separation of yeast (Pethig et al, 1994)
- ❖ Cell fission of sea urchin eggs (Marszalek & Tsong, 1995)
- ❖ Cell fussion (Matsuda et al., 1979)

– Viruses

- ❖ Separation of tobacco mosaic virus and herpes simplex virus (Morgan et al, 1999)

– DNA

- ❖ Increase resolution of DNA fractionatoin or sequencing
- ❖ Enhance in-situ hybridization

– Protein

- ❖ Protein capture/preconcentration

– Latex beads

- ❖ DEP ratchet (Silberzan et al, 1998)

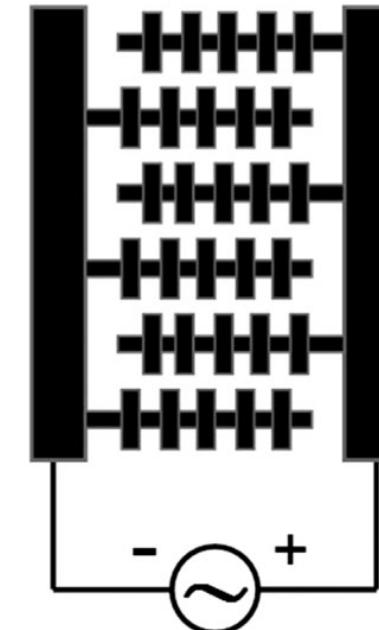


Typical electrode geometries for MDEP

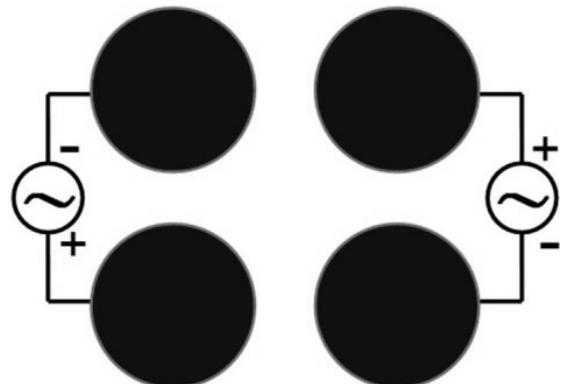
2-D simple gap electrodes



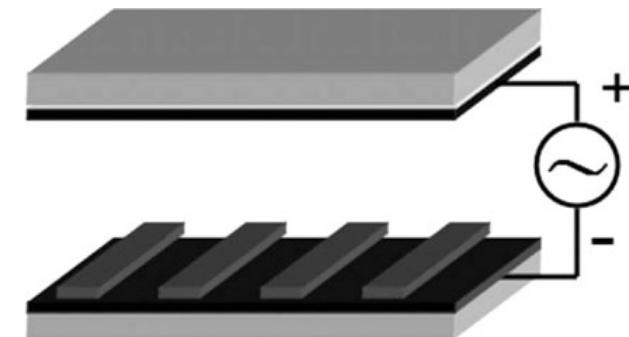
2-D interdigital electrodes



2-D quadruple electrodes

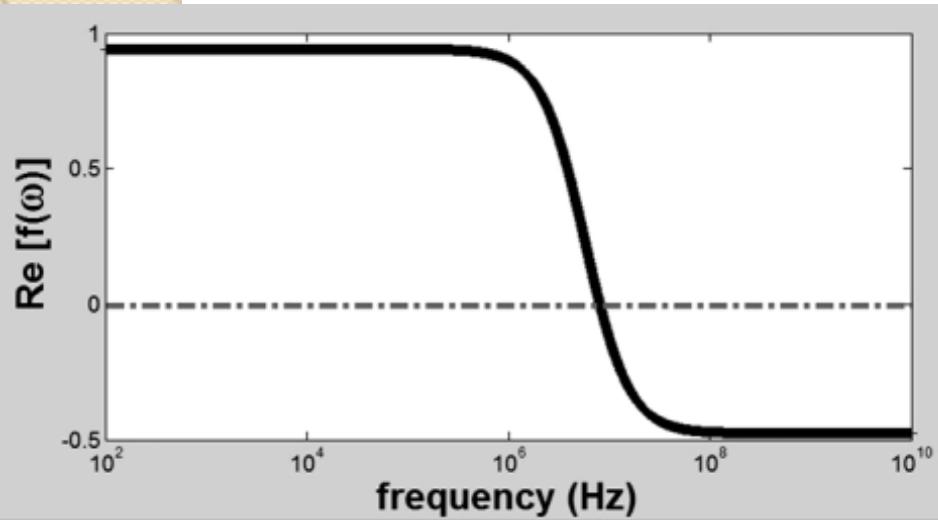


3-D vertical electrodes



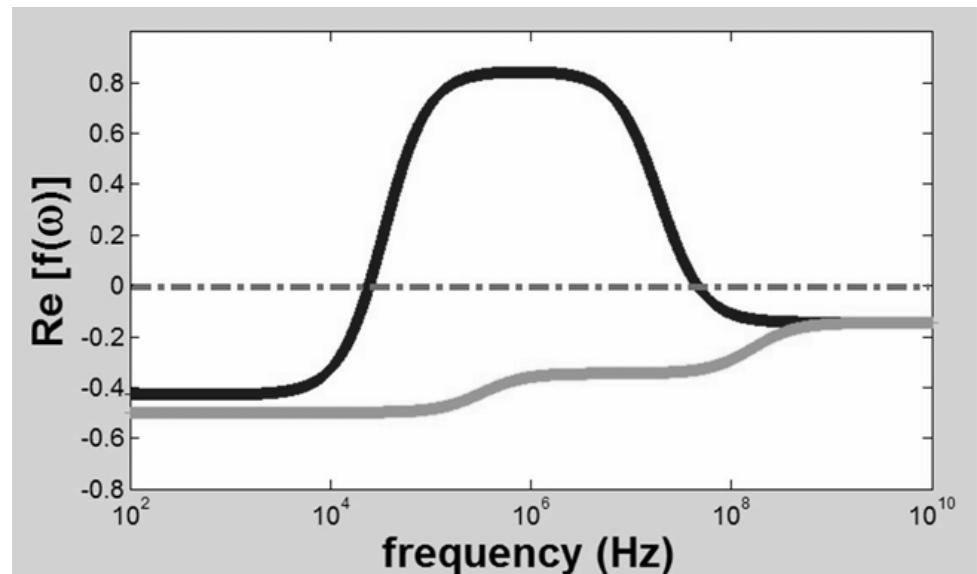


DEP spectrum



The normalized DEP spectrum of $\text{Re}[f_{cm}(\omega)]$ as a function of frequency for a homogenous particle.

The frequency-dependent DEP spectrum for a mammalian cell using a single-shell model.

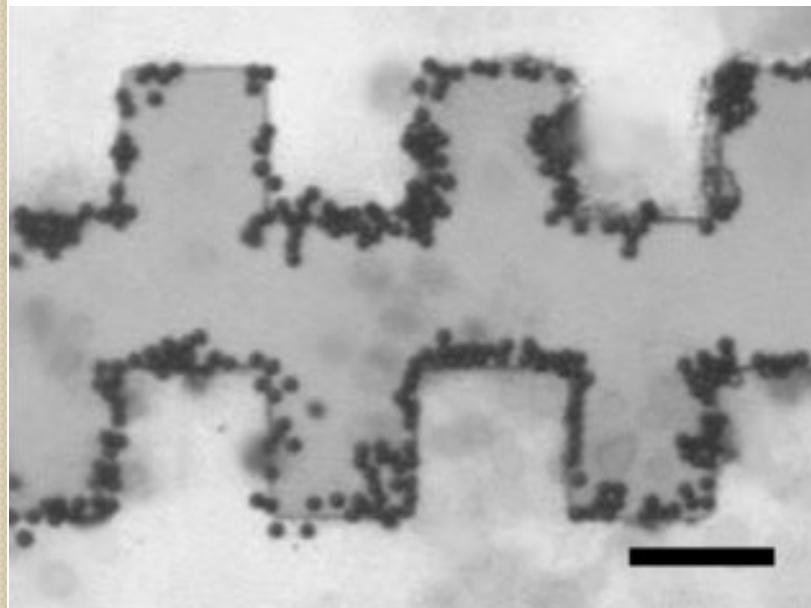


RZ Lin, CT Ho, CH Liu and HY Chang, DEP based-cell patterning for tissue engineering, Biotechnol. J. 2006, 1, 949–957

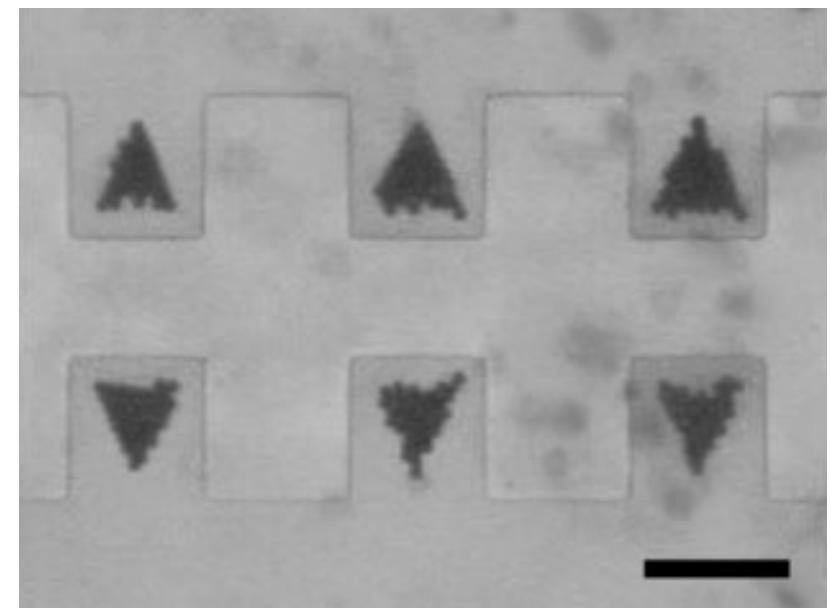


Typical DEP response for particles

Positive DEP of $7\text{-}\mu\text{m}$ polystyrene beads



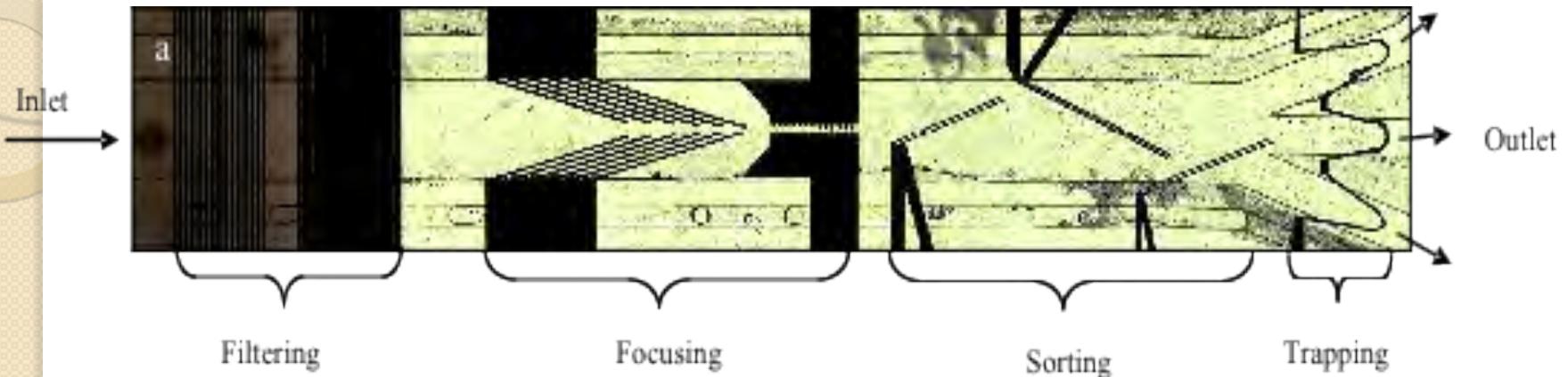
Negative DEP of polystyrene beads



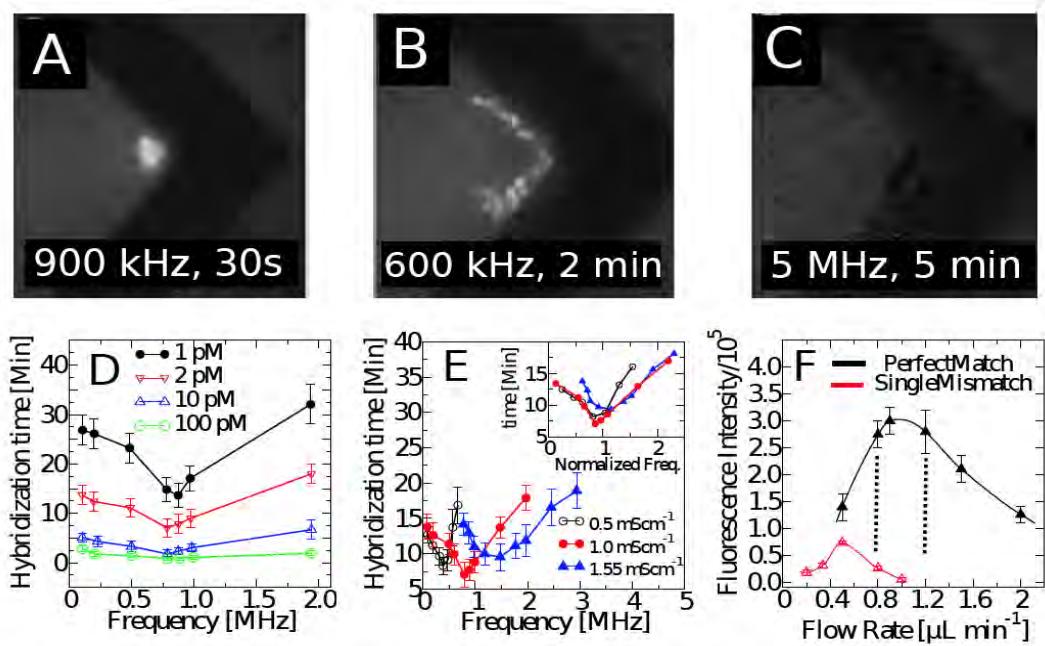
RZ Lin, CT Ho, CH Liu and HY Chang, DEP based-cell patterning for tissue engineering,
Biotechnol. J. 2006, 1, 949–957

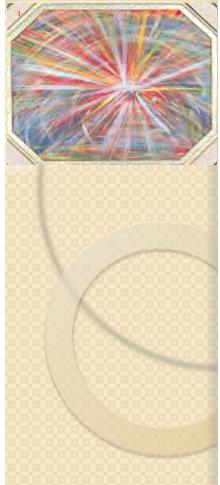


Shear & DEP enhanced CNT sensor



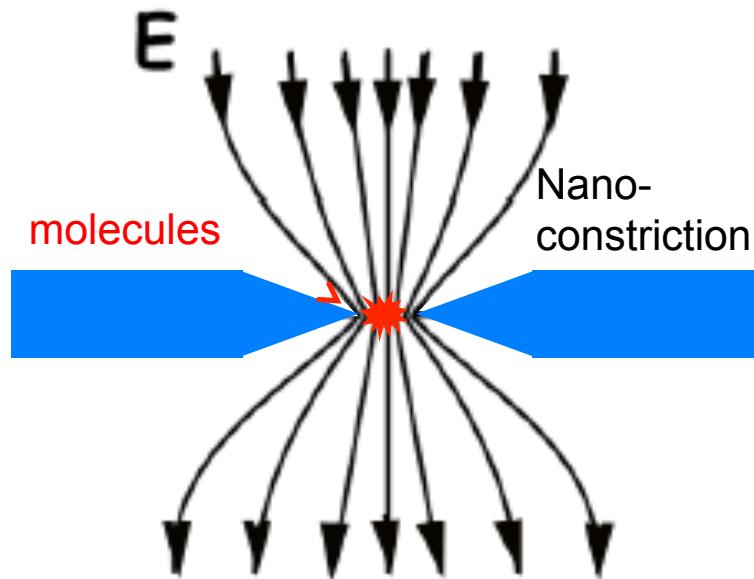
Basuray, S., S. Senapati, et al. (2009). "Shear and AC Field Enhanced Carbon Nanotube Impedance Assay for Rapid, Sensitive and Mismatch-Discriminating DNA Hybridization." *ACS Nano* 3: 1823.





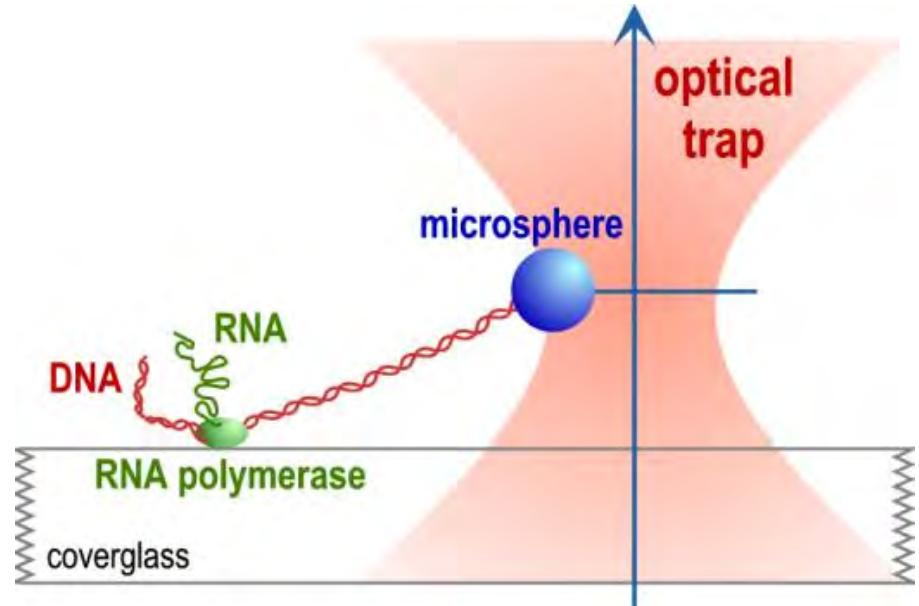
EDEP Molecular Trap vs. Optical Trap

EDEP molecular trap

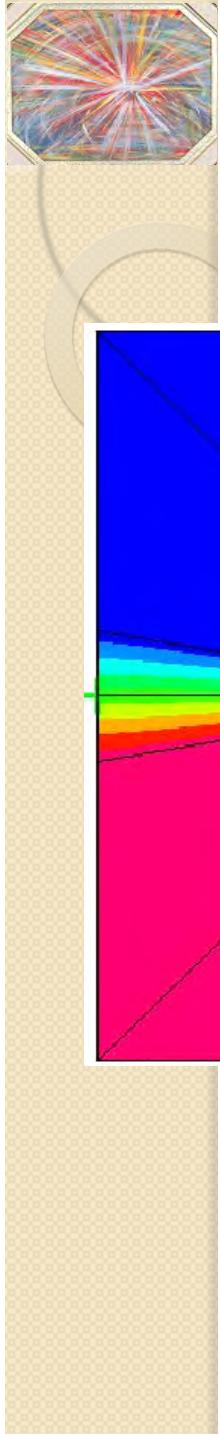


Electric field focused
at the constriction

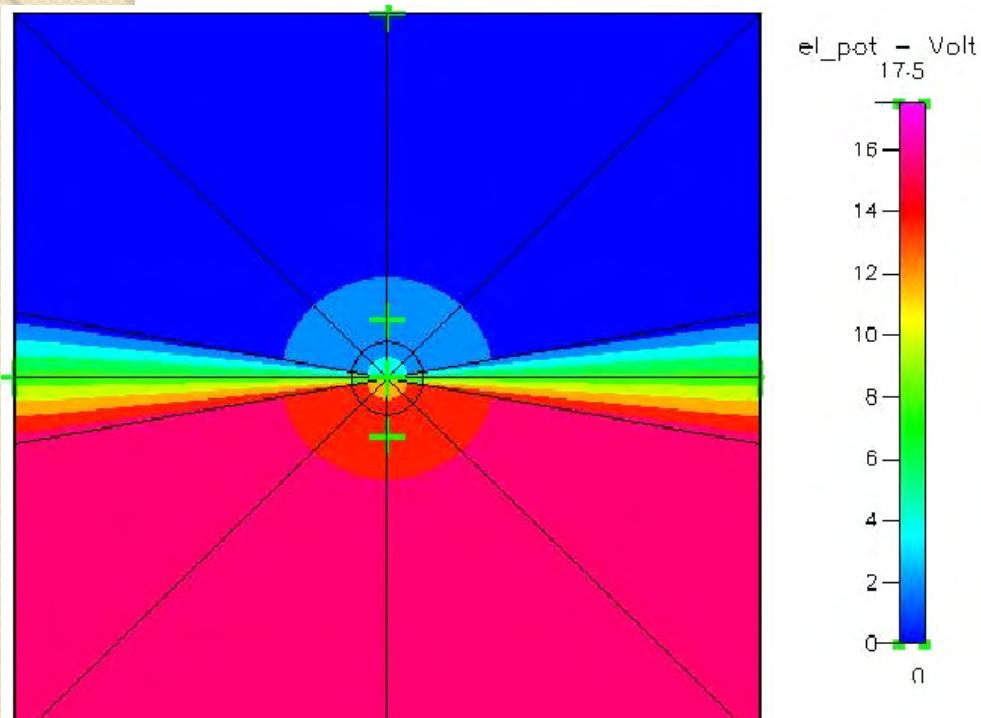
Optical trap



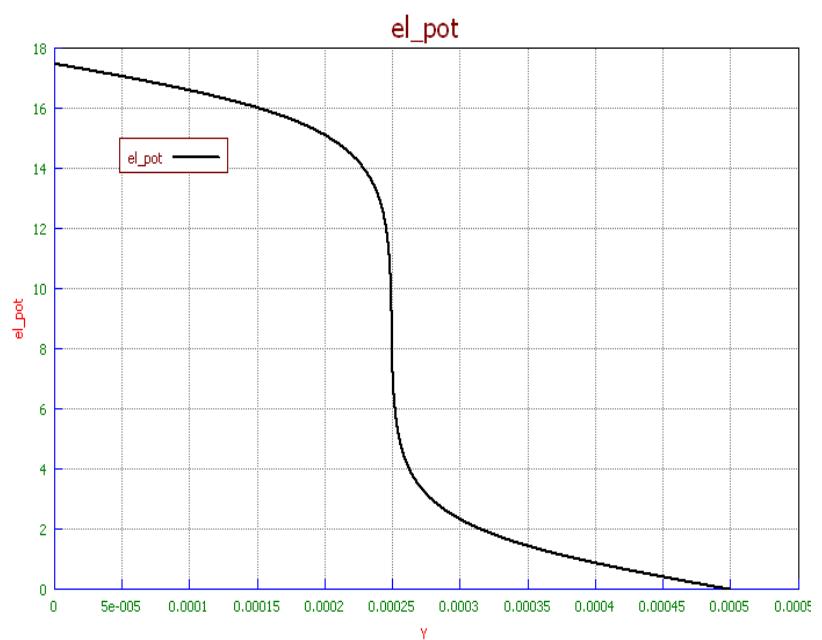
Electric field focused
at the focal point



Electric Potential Distribution

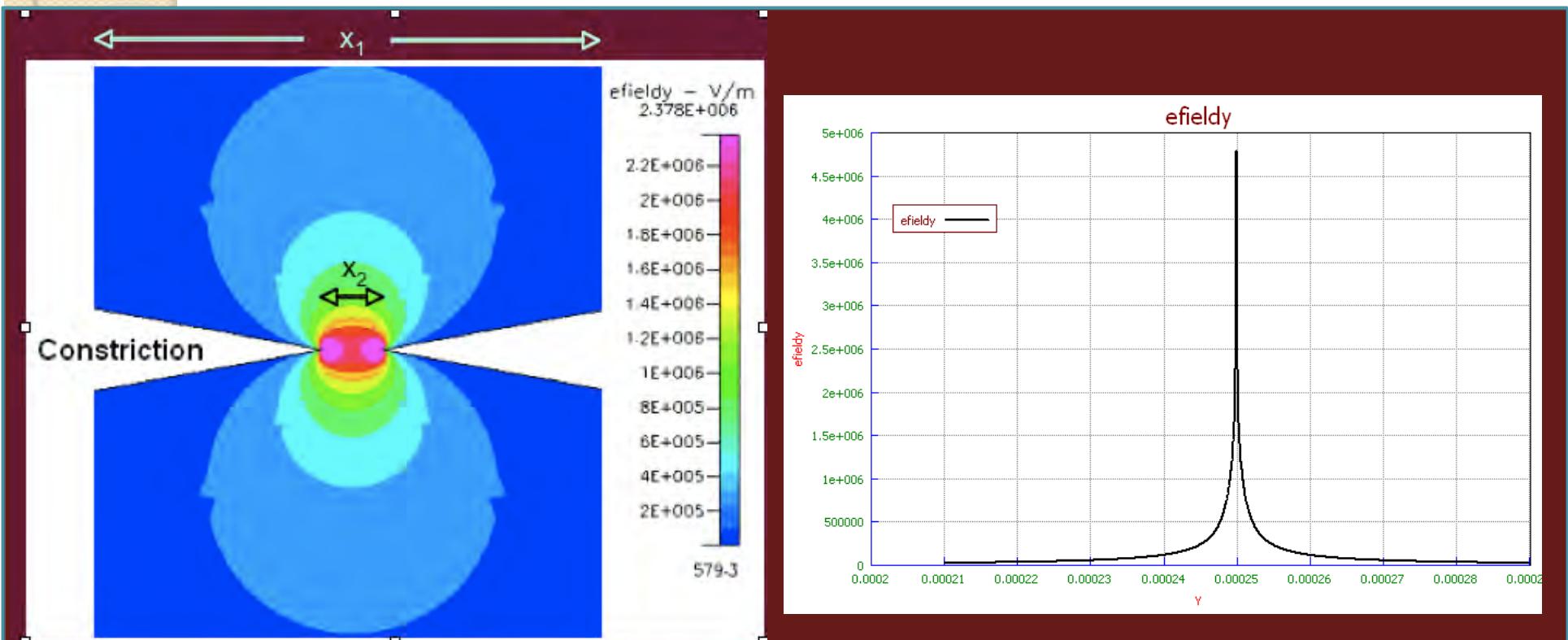


Potential drop mostly occurs at the constriction





Electric Field Enhancement



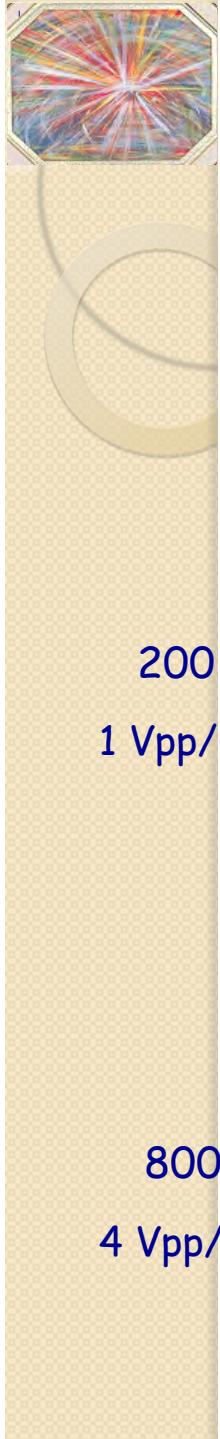
Field focusing factor: $(x_1/x_2)(z_1/z_2)$

For 50 μm /50 nm:

$$E \rightarrow 10^3 x$$

$$\nabla(E^2) \rightarrow 10^6 x$$

Field focusing mostly occurs at the (tips of) constriction



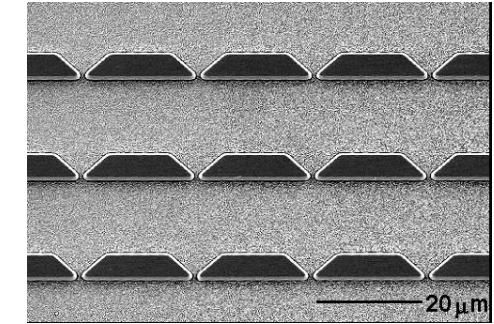
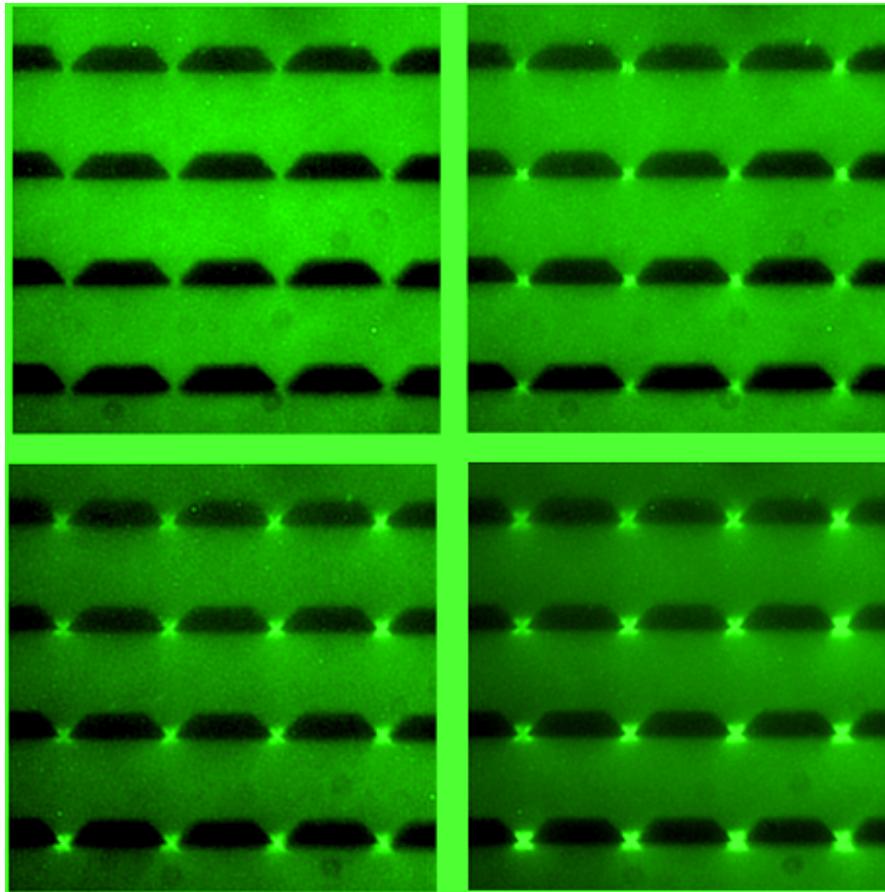
Electrodeless DEP for DNA concentration

–Field response at a fixed frequency

368bp, 1000 Hz in 0.5xTBE

▲
E
▼
200 Vpp/cm
1 Vpp/unit cell

800 Vpp/cm
4 Vpp/unit cell



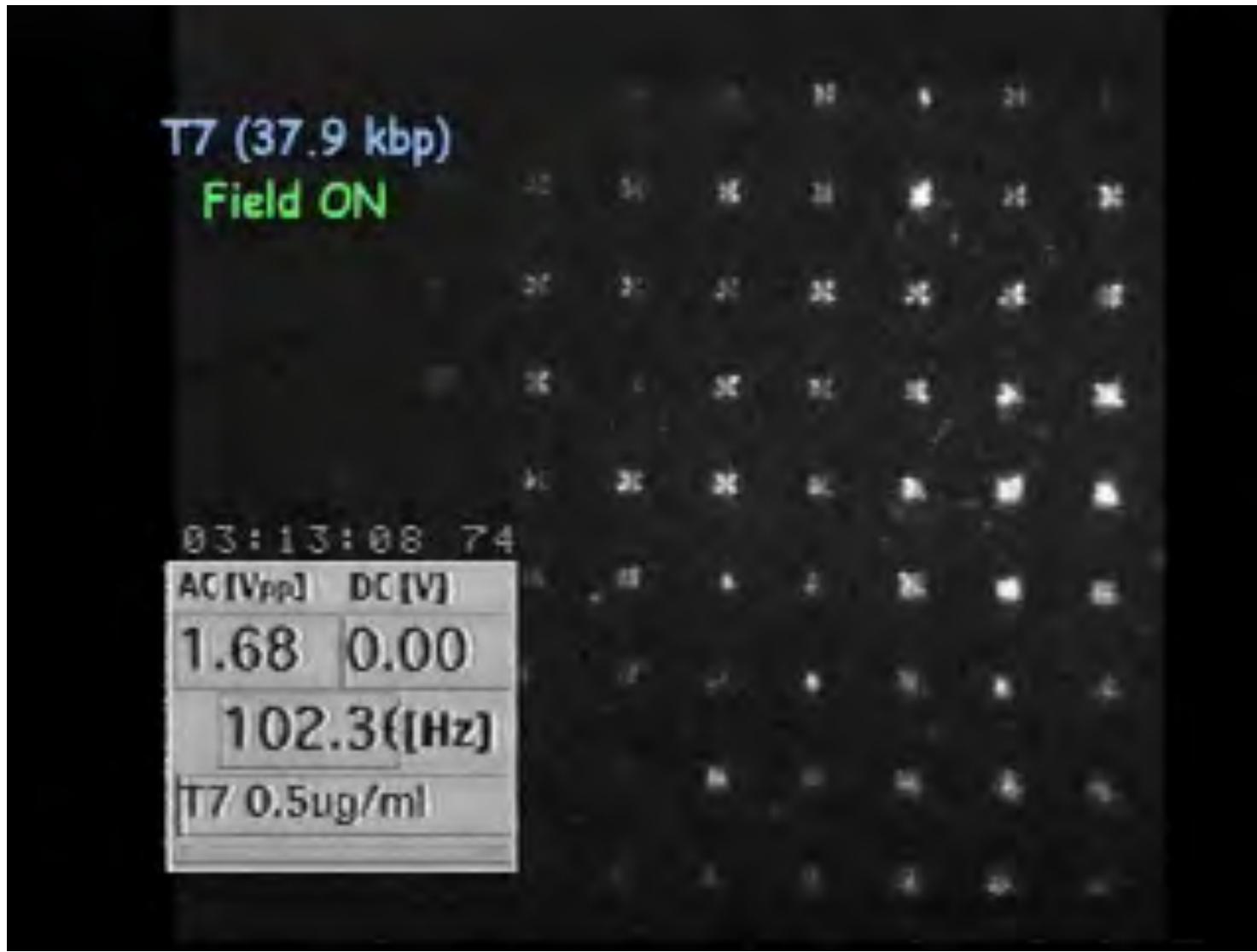
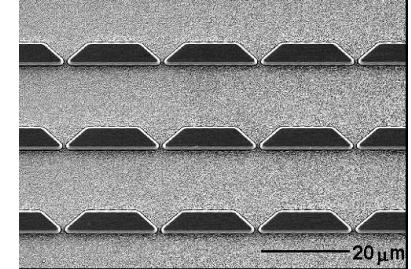
400 Vpp/cm
2 Vpp/unit cell

1000 Vpp/cm
5 Vpp/unit cell

Chou et al., Biophys. J. 83: 2170-2179 (2002)
US Patent # 6,824,664 (2004)

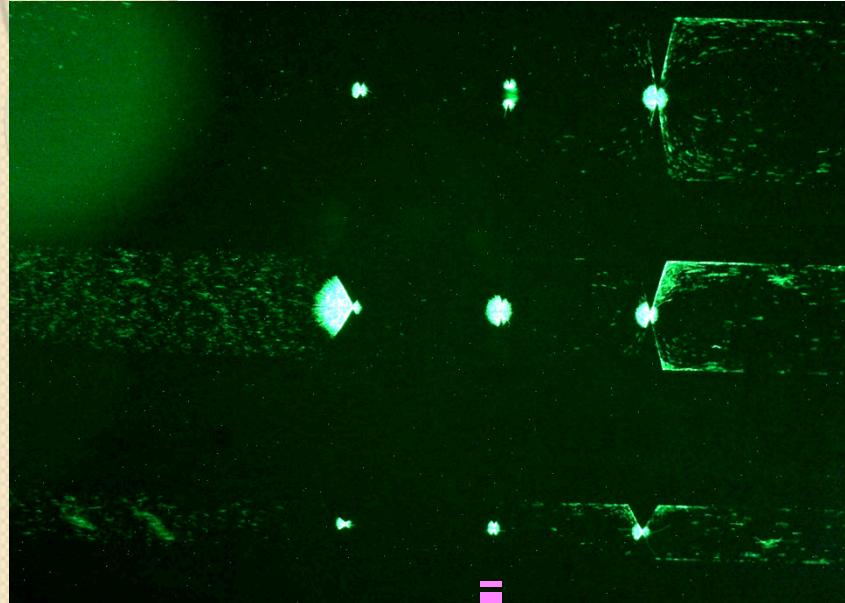


EDEP-Trapping of DNA (movie)

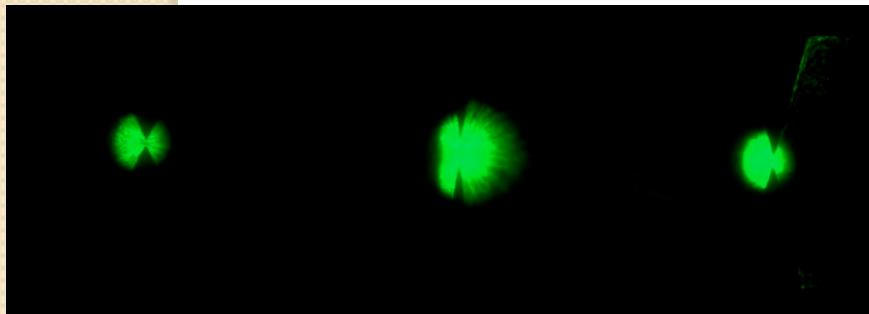




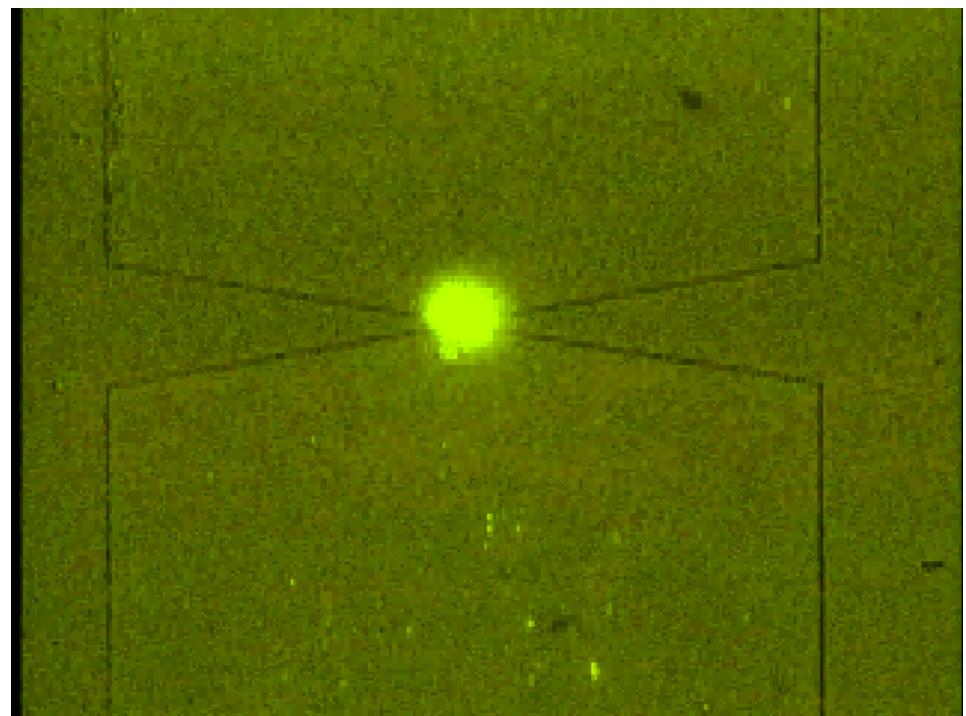
EDEP Array for Cell *E. coli* Trapping



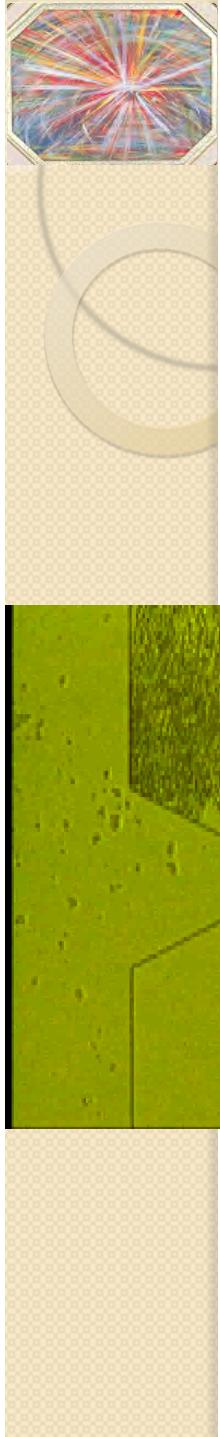
Enrichment $\sim 10^{3-4}$



4 μm constriction,
10 μm deep
50-2 MHz, 100Vpp/cm
Buffer salt concentration:
up to 100 mM



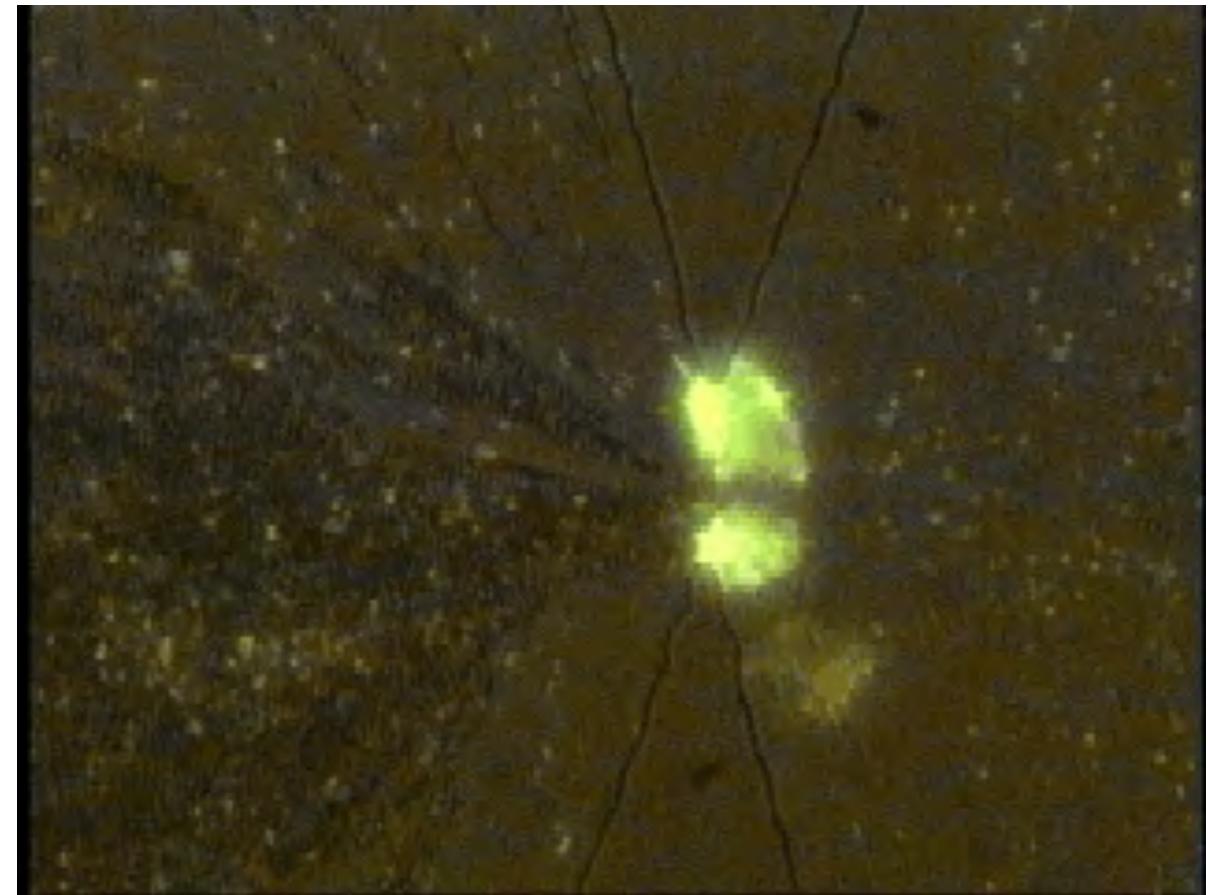
C. F. Chou, F. Zenhausern (2003) IEEE Eng. Med. Biol. Mag. Nov/Dec. 62-67.



EDEP Array for Cell Separation

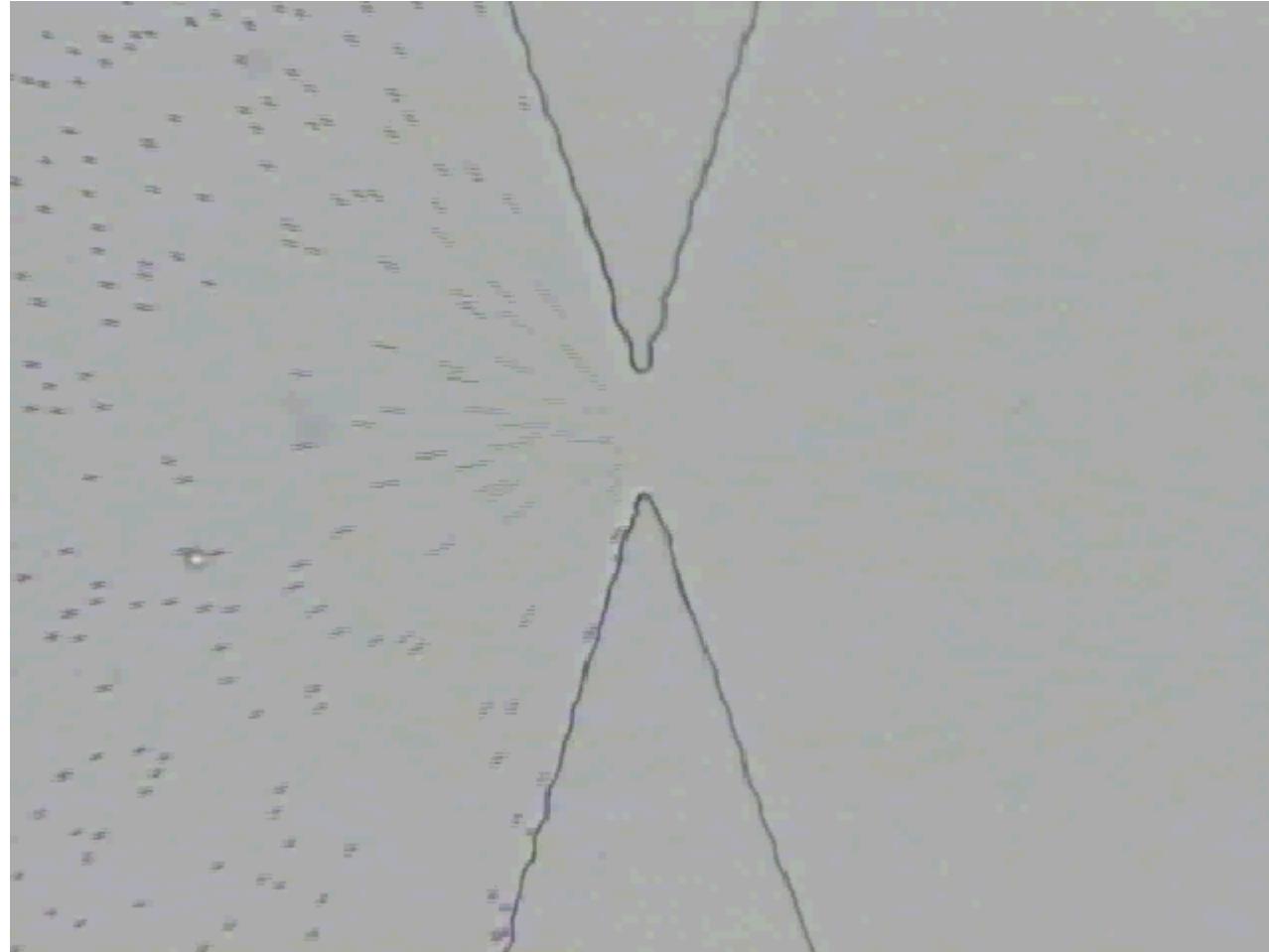
Device: PDMS/glass

RBC (- DEP) and *E. coli* (+ DEP)

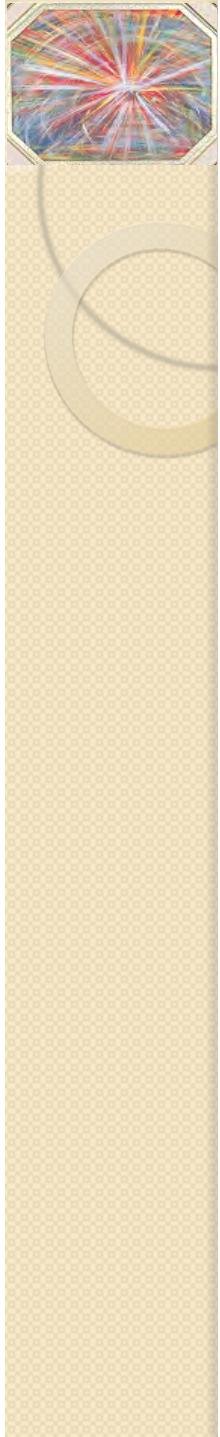




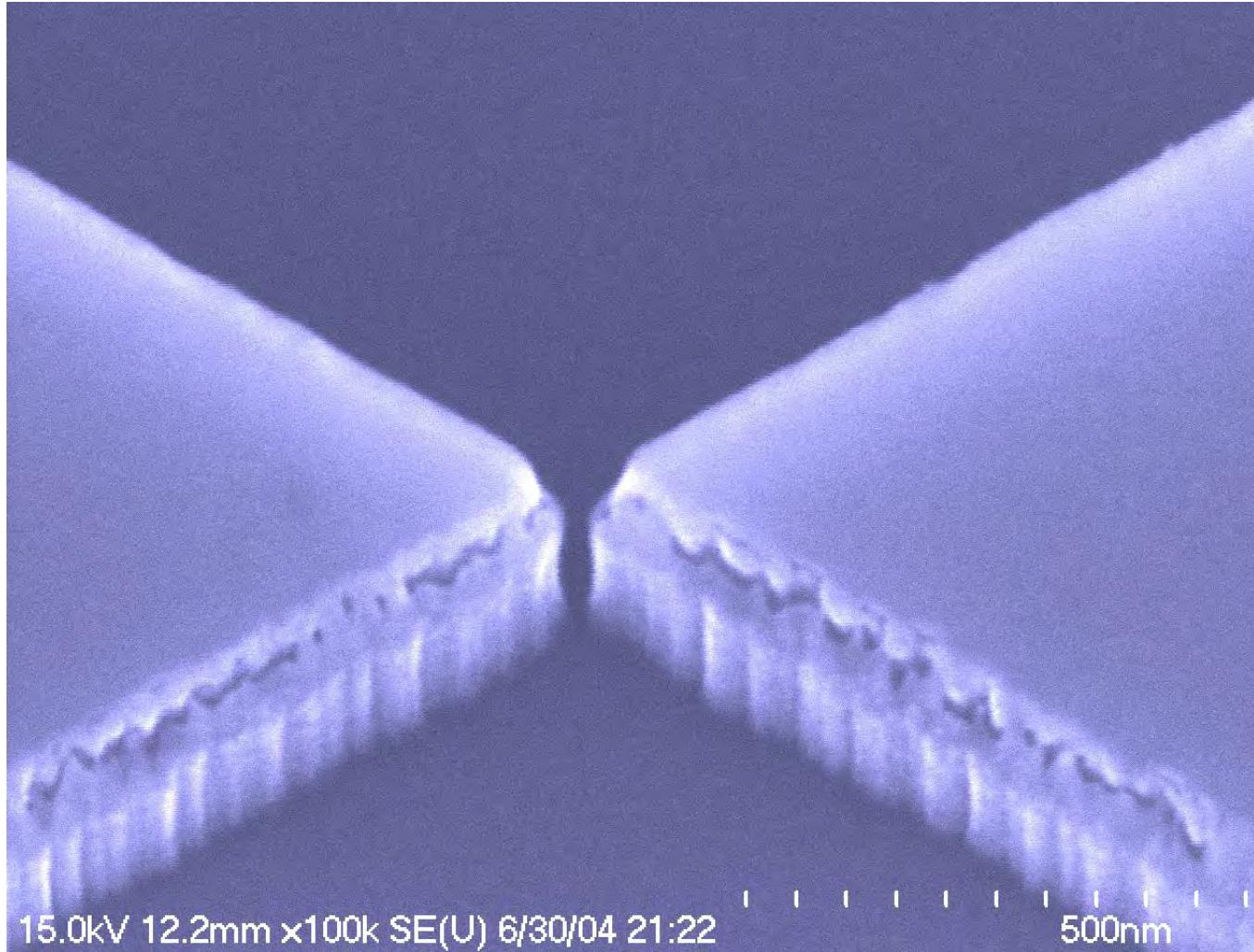
High field for cell lysing



C. F. Chou, F. Zenhausern (2003) IEEE Eng. Med. Biol. Mag. Nov/Dec. 62-67.



Nanoscale protein trap

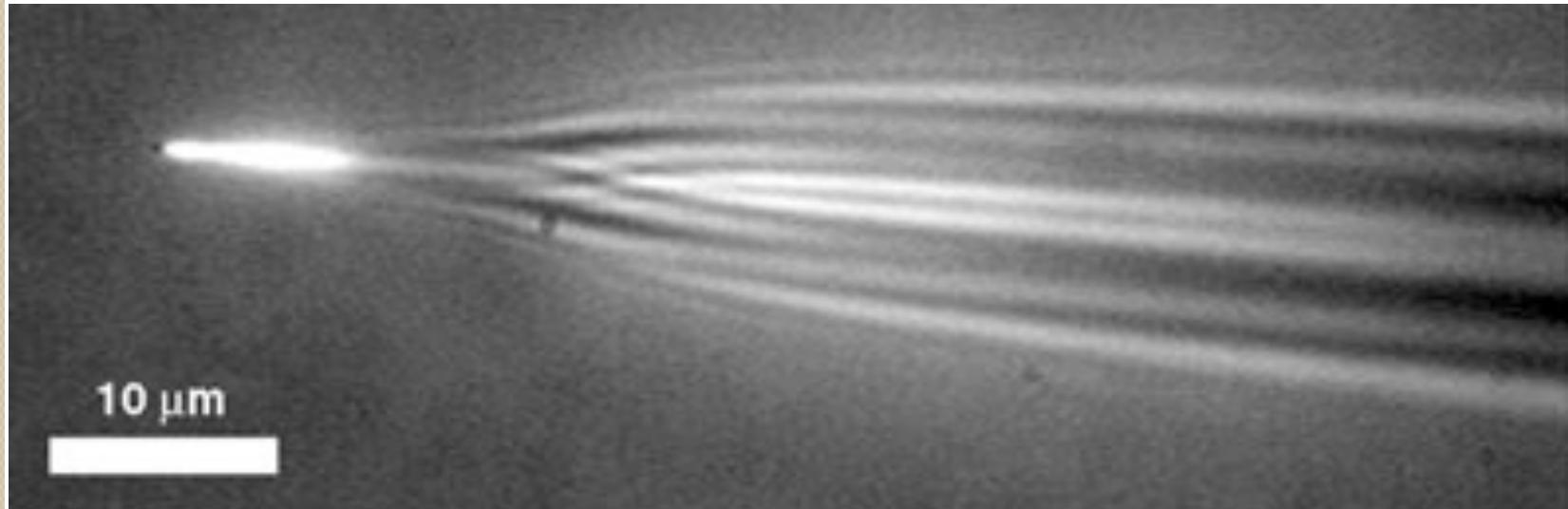


50 nm gap/250 nm deep



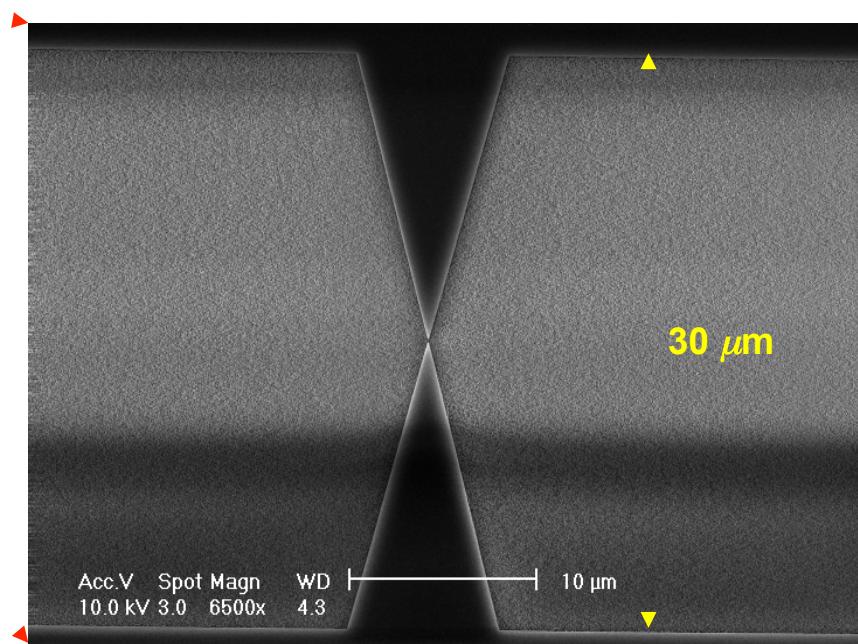
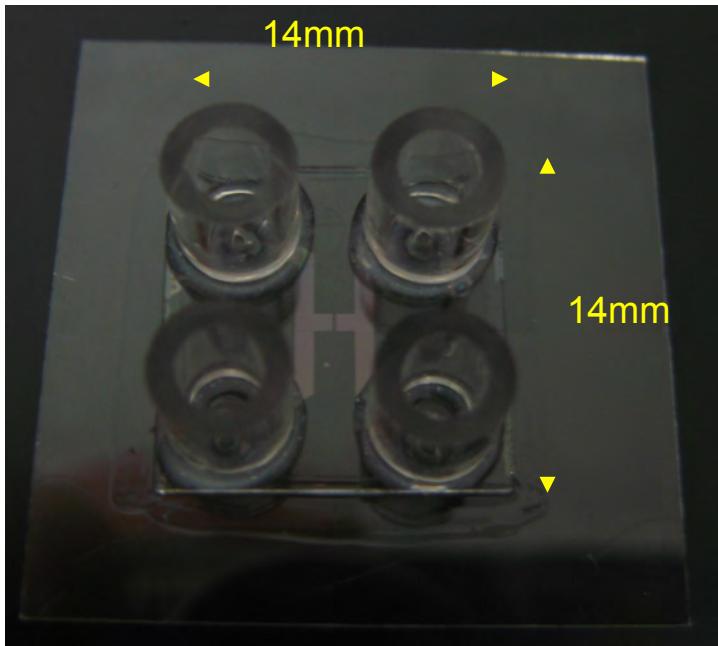
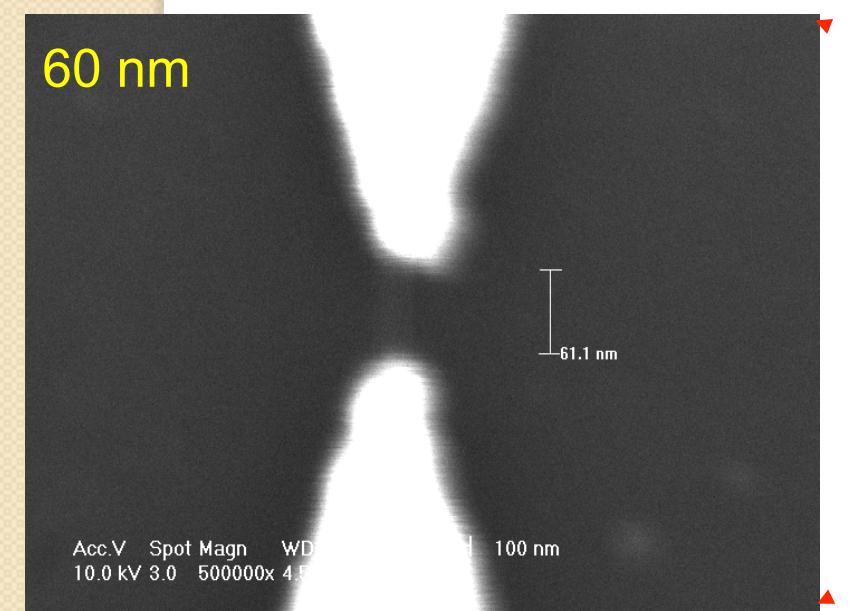
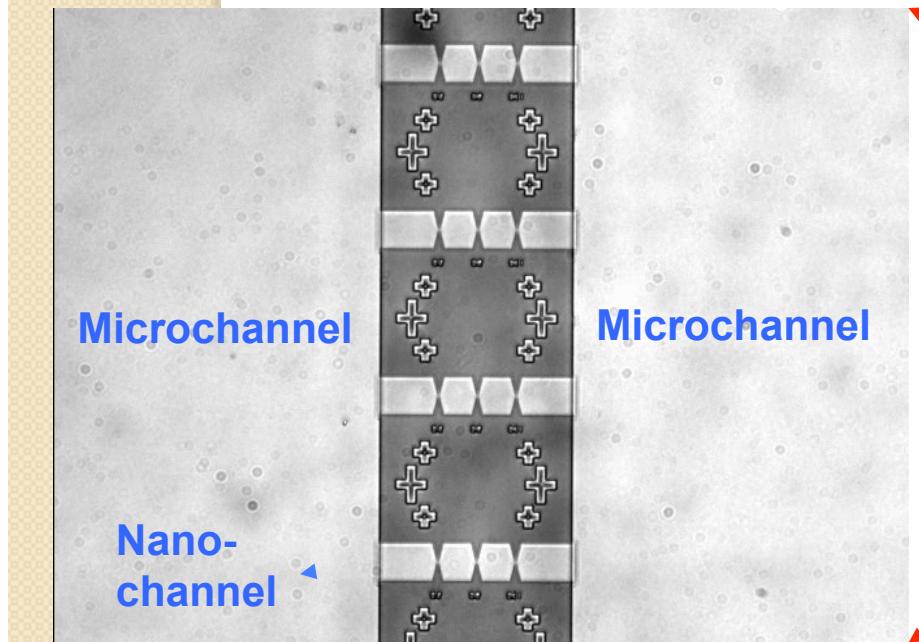
Protein trapping using nanopipette

10^3 -fold enhancement in seconds



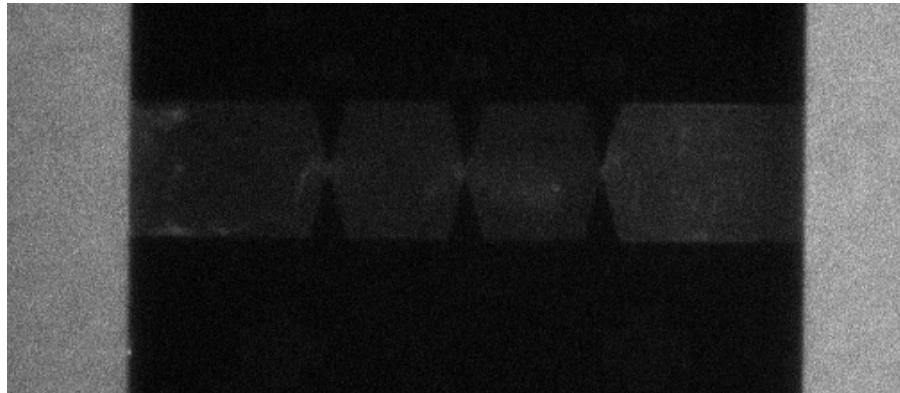
RW Clarke et al., Angew. Chem. Int. Ed. 44, 3747 (2005)

Nanoscale protein trap

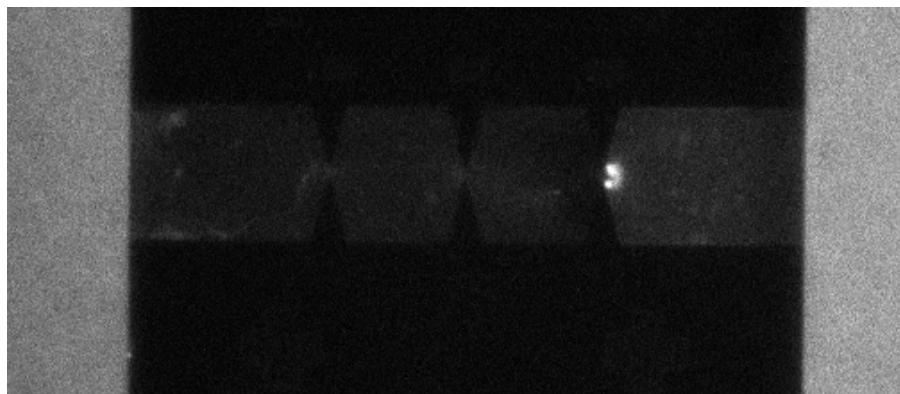




Negative DEP for protein enhancement



$t = 0 \text{ sec}$



$t = 0.1 \text{ sec}$

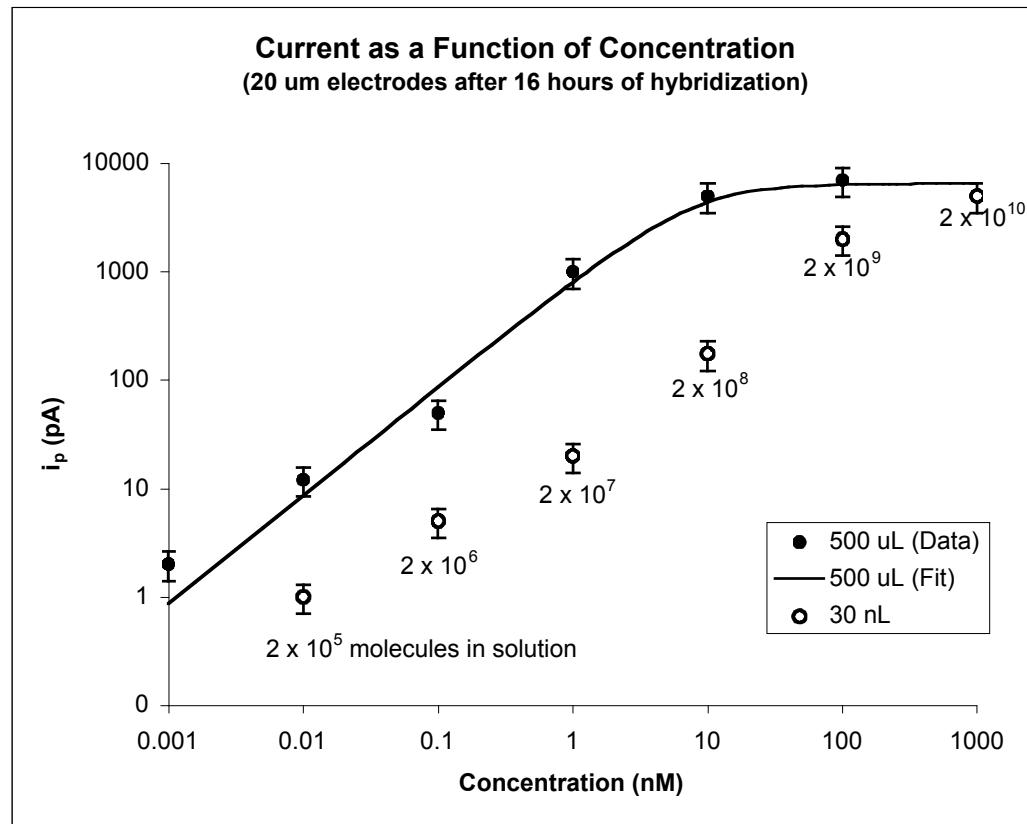


$t = 0.8 \text{ sec}$



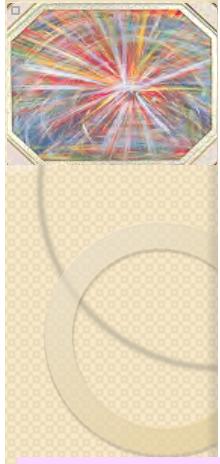
Why molecular traps?

Titration of detection limit with microelectrodes in microchamber



N. Swami

This data set demonstrates a chief bottleneck for *all* miniaturized sensing methods in general, and surface binding assays in particular. This is associated with the chemical kinetic limits to sensitivity upon miniaturization. → Solution: sample pre-concentration!!



DEP applications on DNA/protein sensors

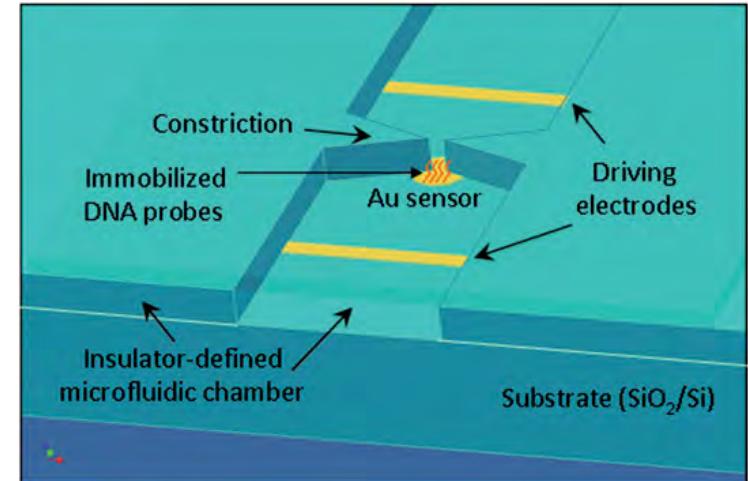
Hybridization kinetics enhancement by sample preconcentration

Second order kinetics: $Ct_{1/2} = I/k$

C = probe concentration (moles/liter)

k = Rate constant

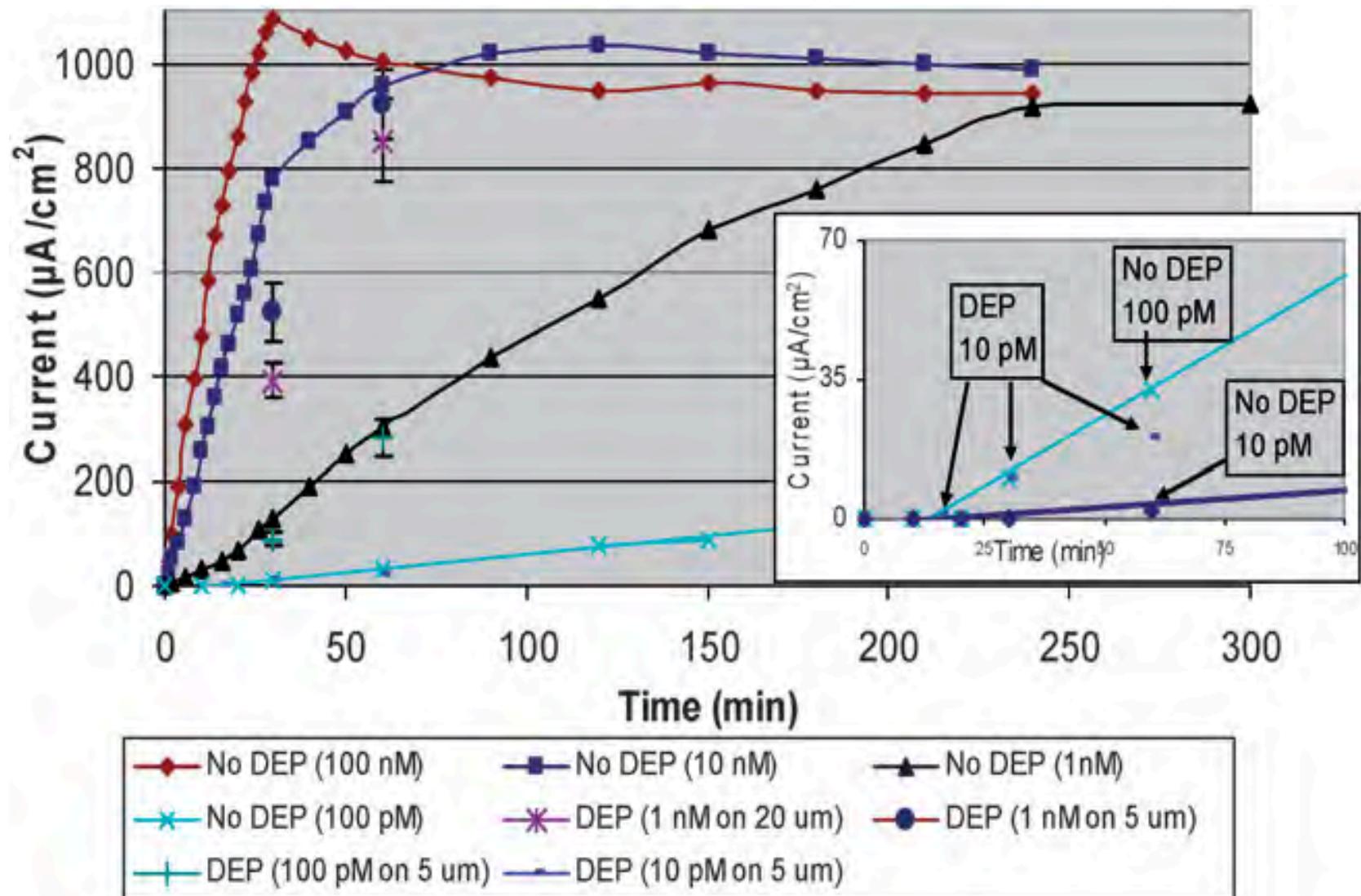
$t_{1/2}$ = the time in seconds it takes for a probe of given concentration to reach 50% annealed.



Concentration enhancement	Annealing time of hybridization		
	50%	75%	95%
1x	10 hrs	30 hrs	100 hrs
100x	6 min	18 min	60 min
1000x	36 sec	1.8 min	6 min



Enhanced DNA sensor kinetics



Swami, N., C.F. Chou, et al. (2009). "Enhancing DNA Hybridization Kinetics through Constriction-Based Dielectrophoresis." *Lab on a Chip* 9: 3212-3220.

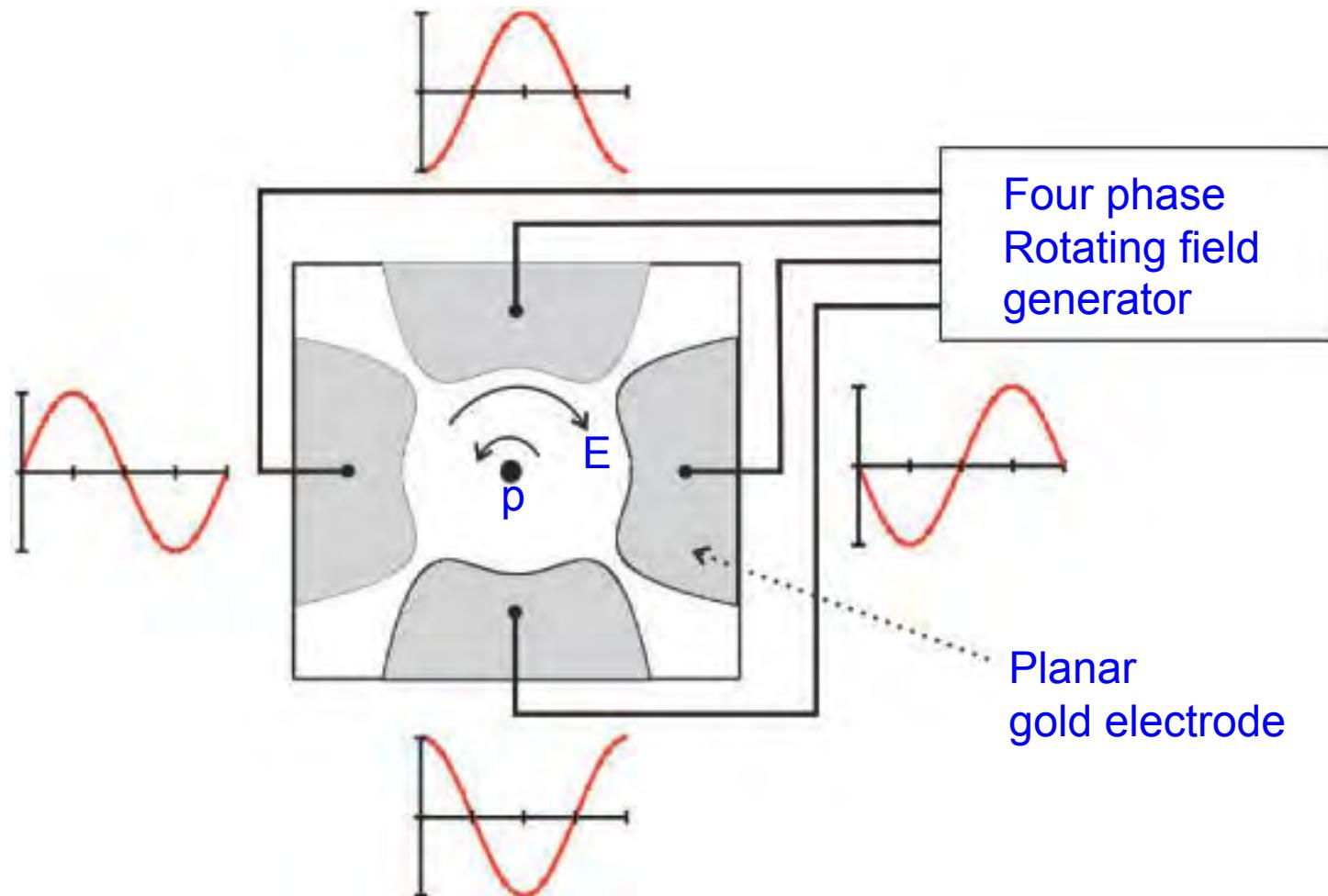


Phenomena associated with DEP:

- Electrorotation and traveling wave DEP (TWDEP)
- Field-flow fractionation DEP (FFF-DEP)
- Optoelectronic tweezers



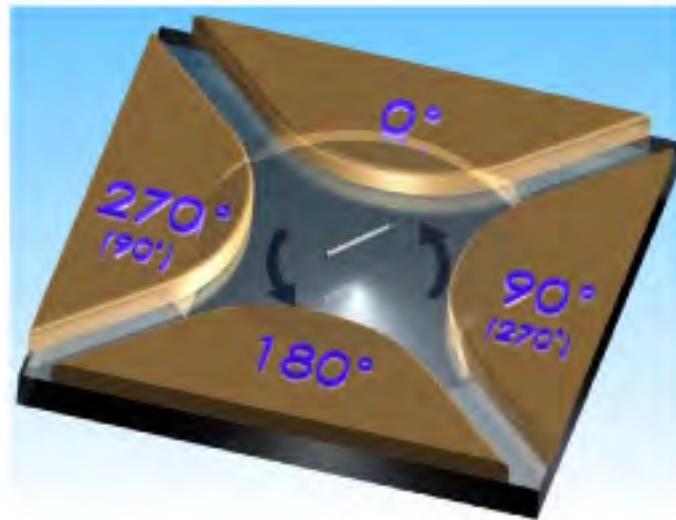
Electrorotation and traveling wave DEP



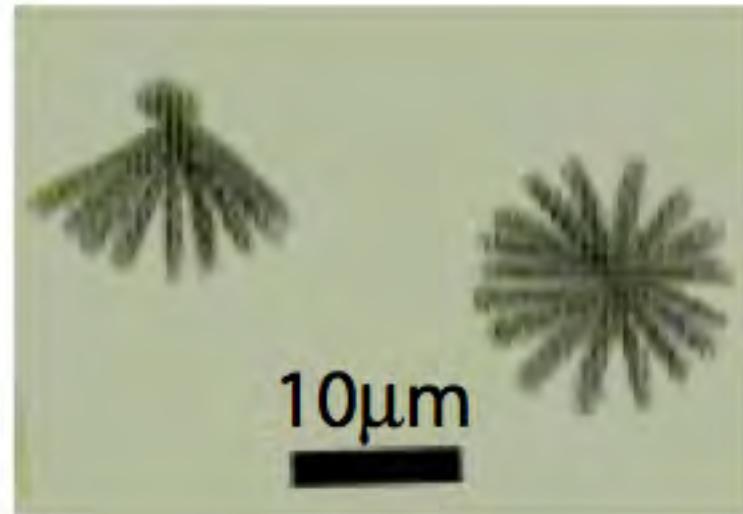


Controllable High-Speed Rotation of Nanowires

(a)



(b)



JHU

Nanowire motor

10 V, 20 kHz

00:00.00

JHU

Au nanowire

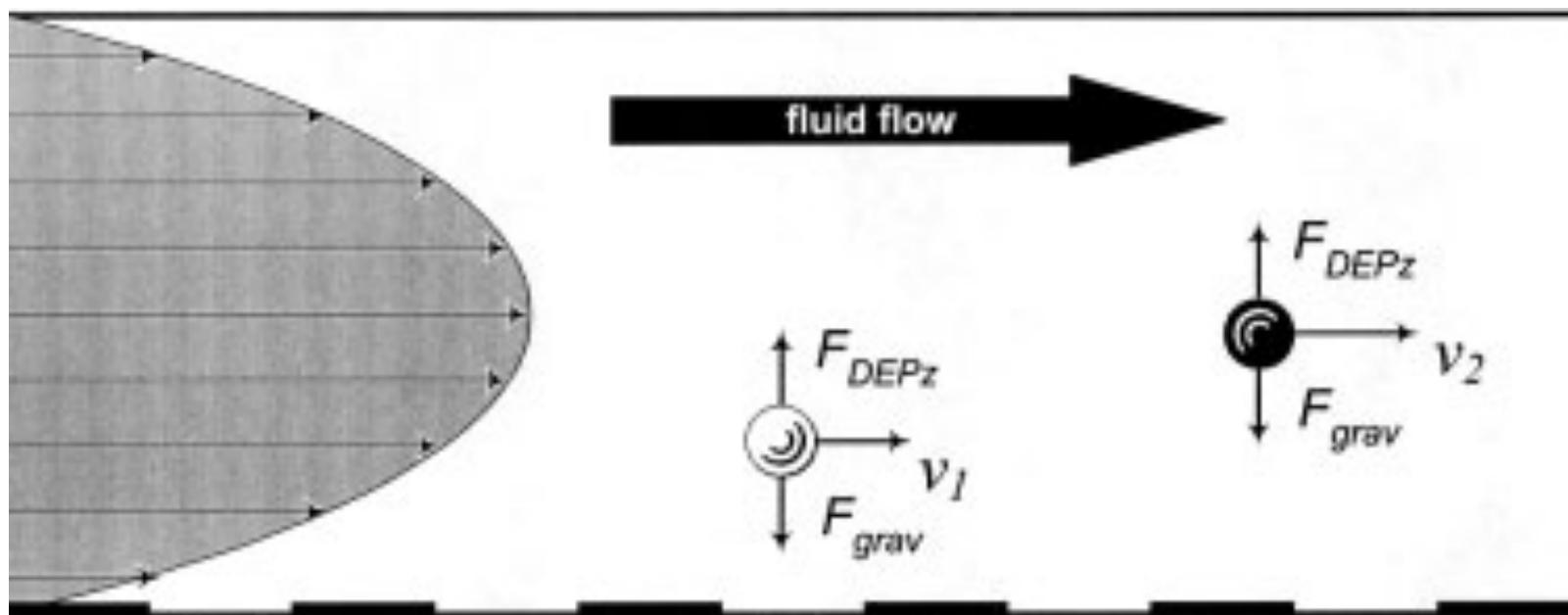
5 V, 5 kHz

00:00.00

D. L. Fan, F. Q. Zhu, R. C. Cammarata, C. L. Chien, *PRL* 94, 247208 (2005)



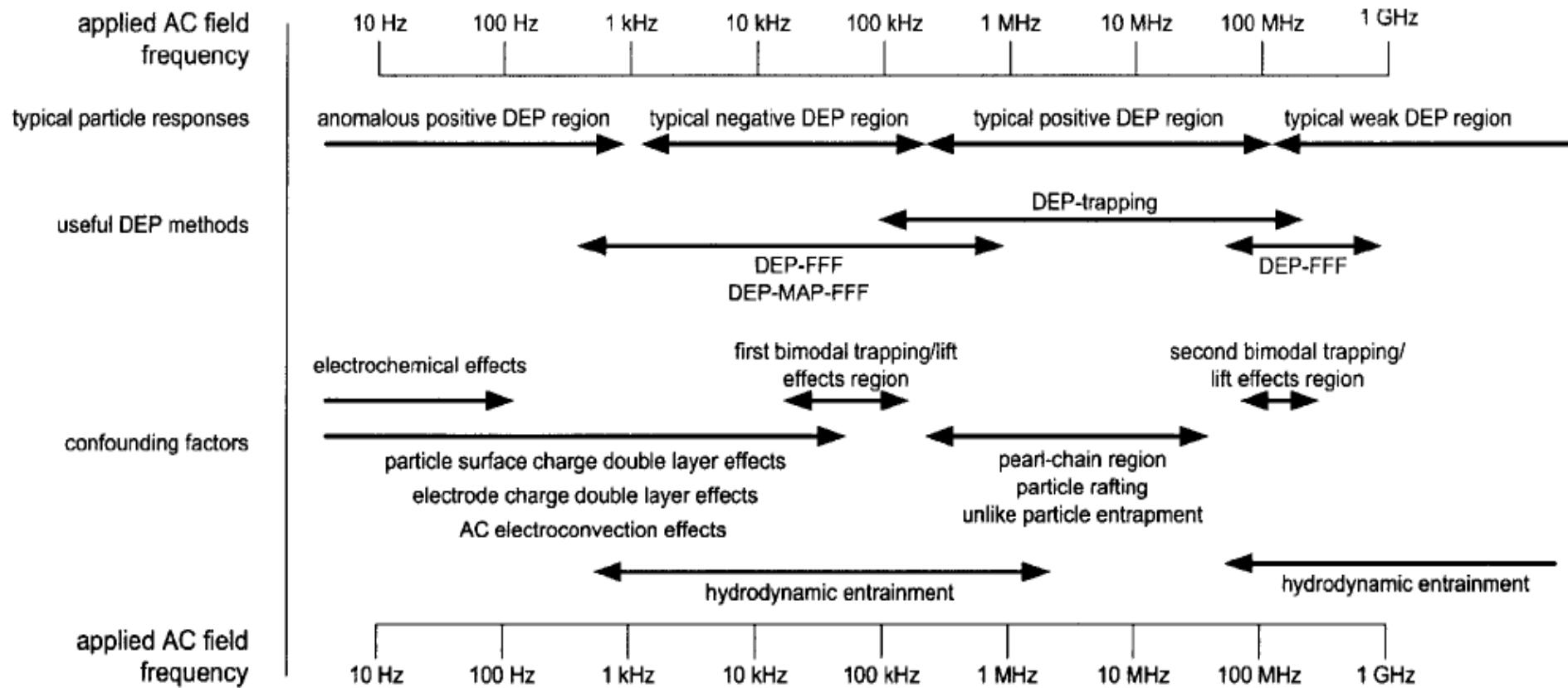
Principle of hyperlayer DEP-FFF



PRC Gascoyne & J Vykoukal, "Particle separation by dielectrophoresis"
Electrophoresis 2002, 23, 1973–1983.



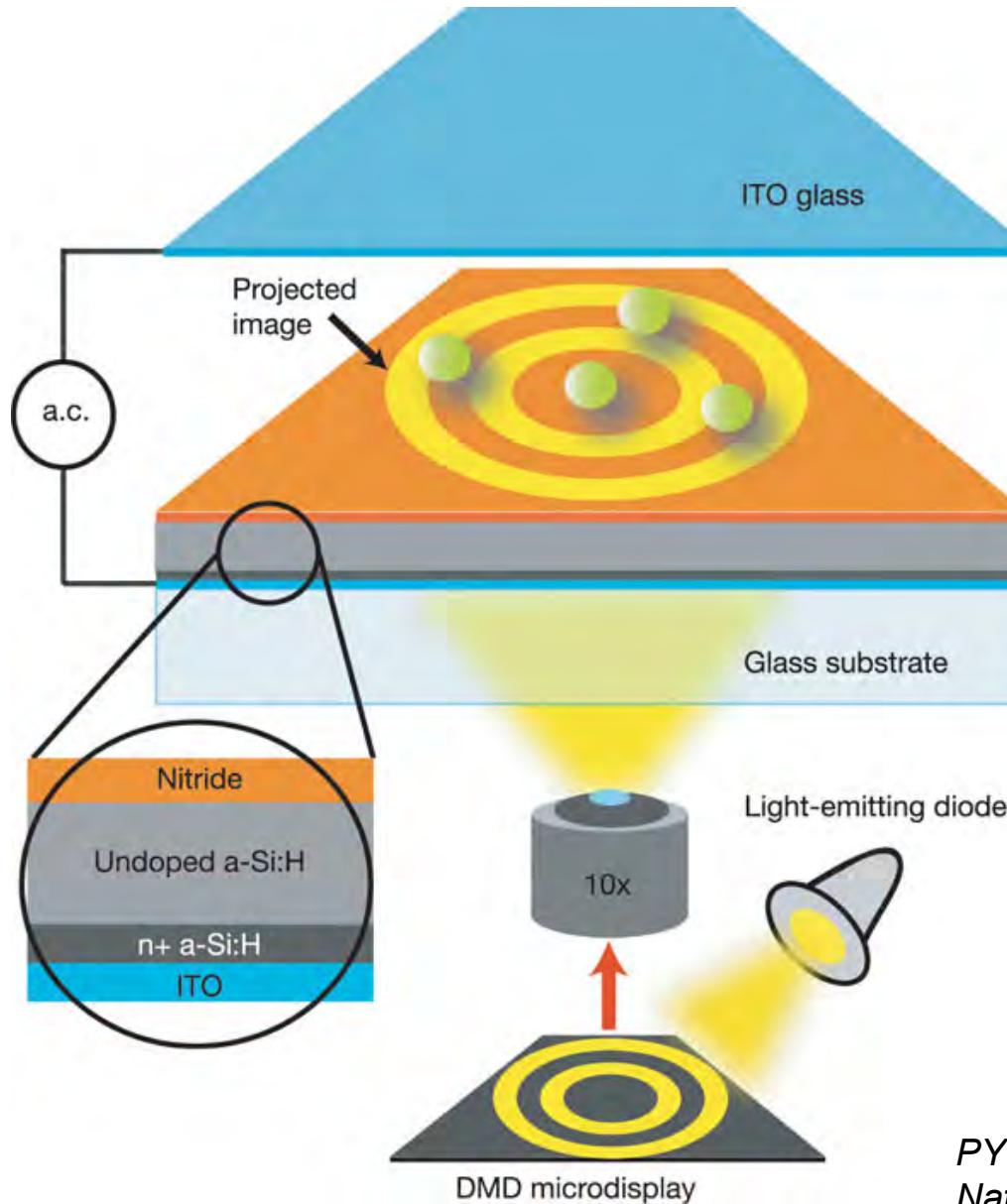
Guide to frequency bands for various DEP phenomena



PRC Gascoyne & J Vykoukal, "Particle separation by dielectrophoresis"
Electrophoresis 2002, 23, 1973–1983.



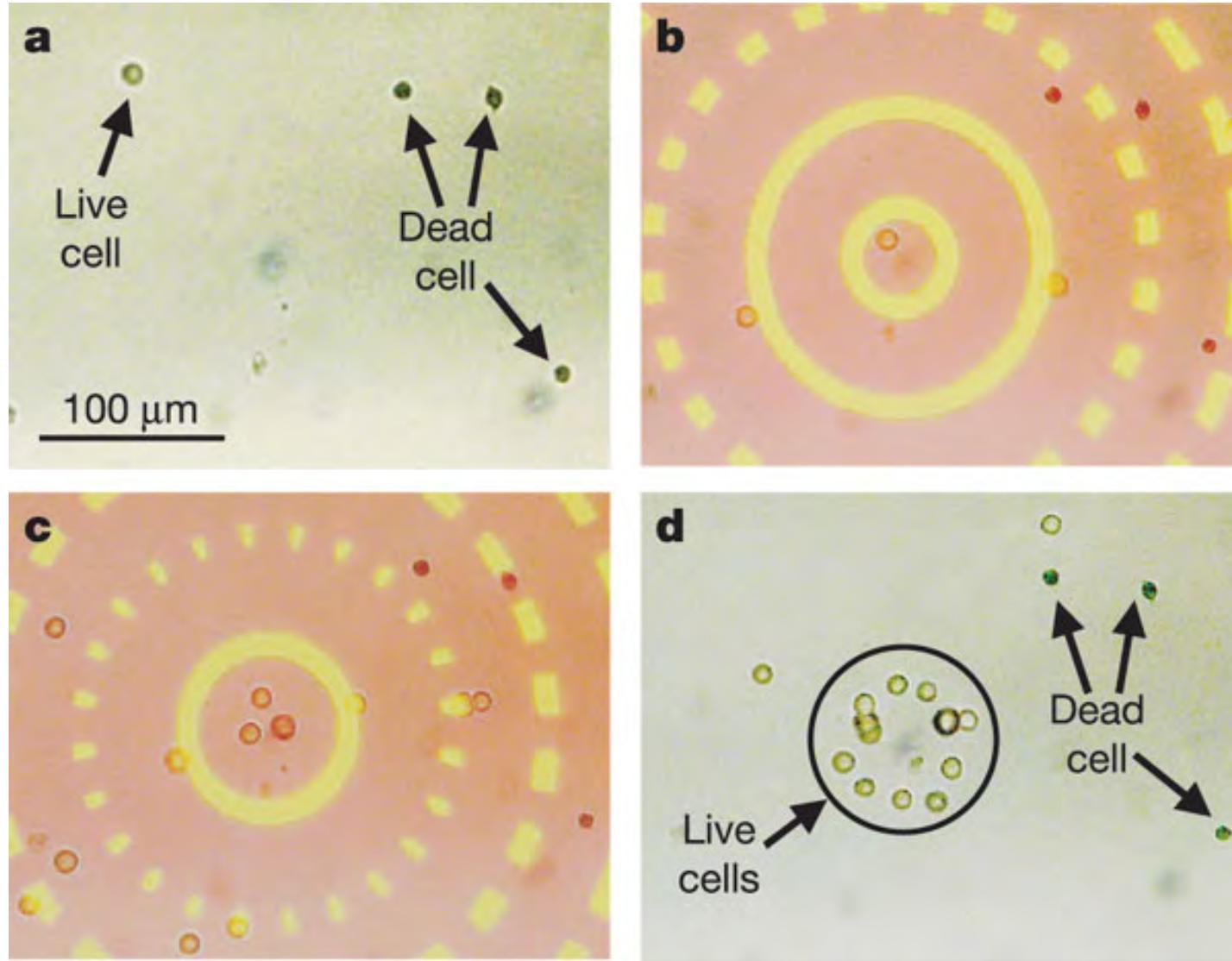
Optoelectronic tweezers



PY Chiou, AT Ohta, MC Wu,
Nature 436, 370-372 (2005)



Optoelectronic tweezers—cell sorting



PY Chiou, AT Ohta, MC Wu, *Nature* 436, 370-372 (2005)

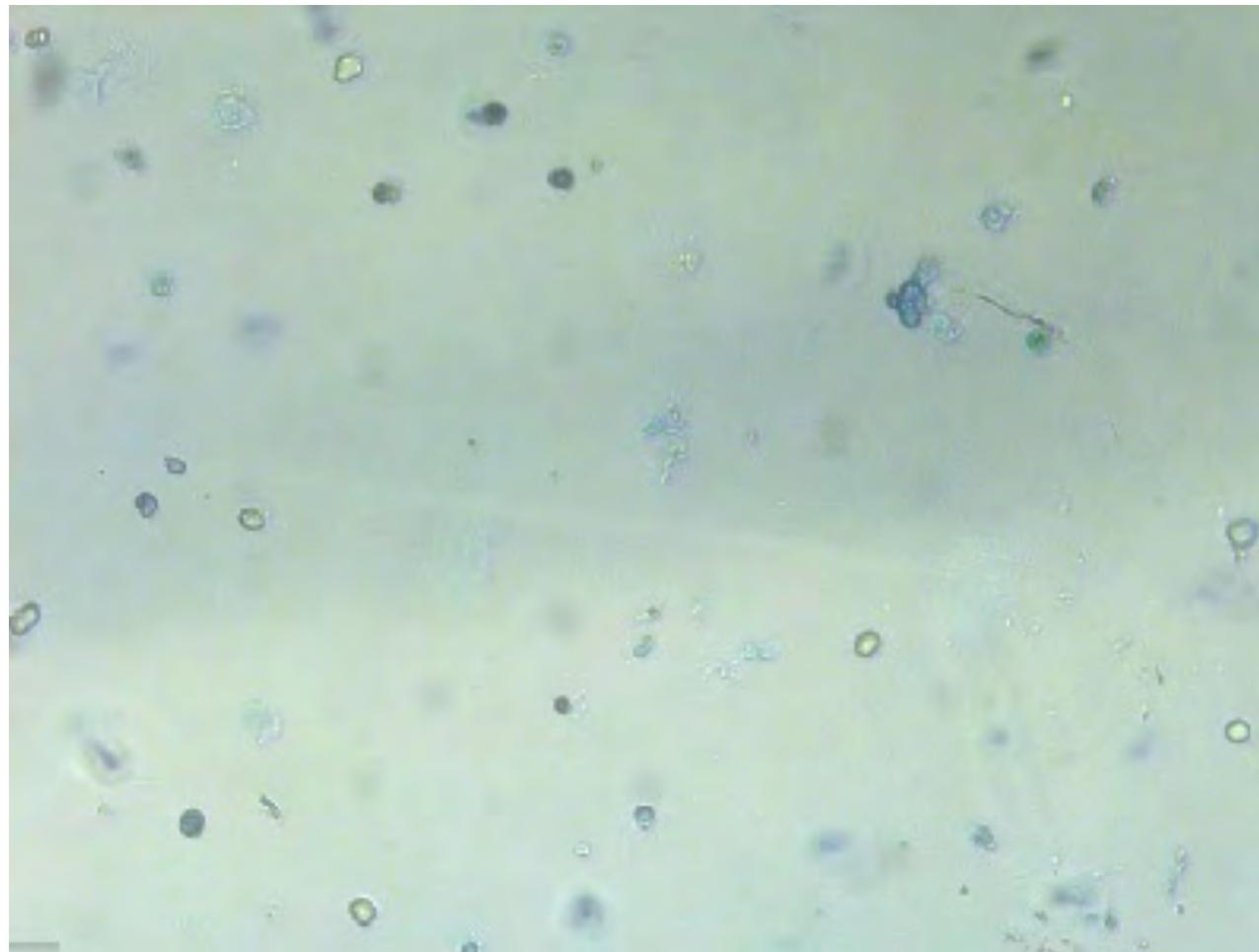


Optoelectronic tweezers

Cell sorting—live & dead cells

The selective concentration of live human B cells is accomplished using positive OET

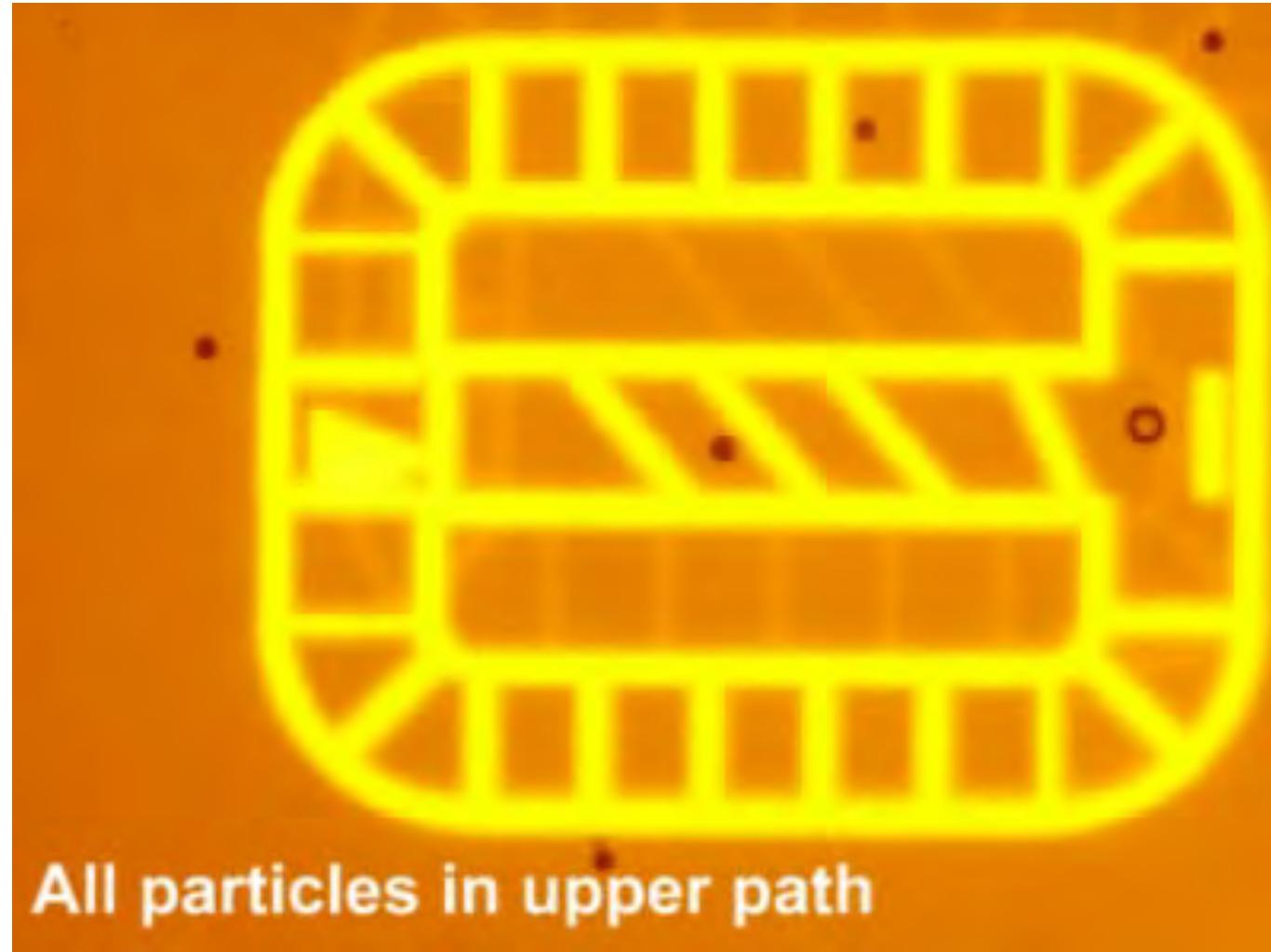
(Movie)



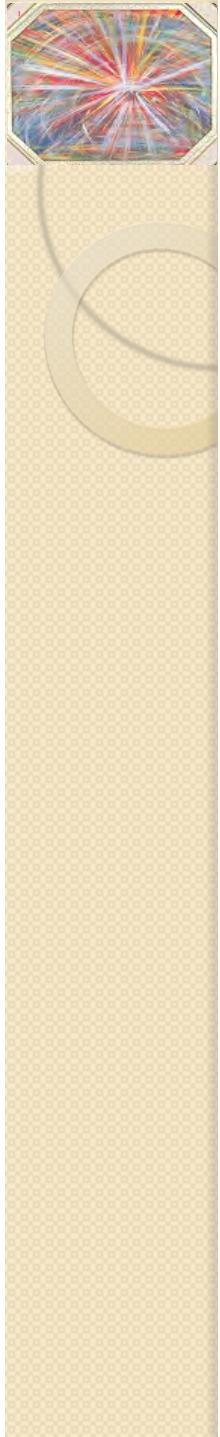
PY Chiou, AT Ohta, MC Wu, *Nature* 436, 370-372 (2005)



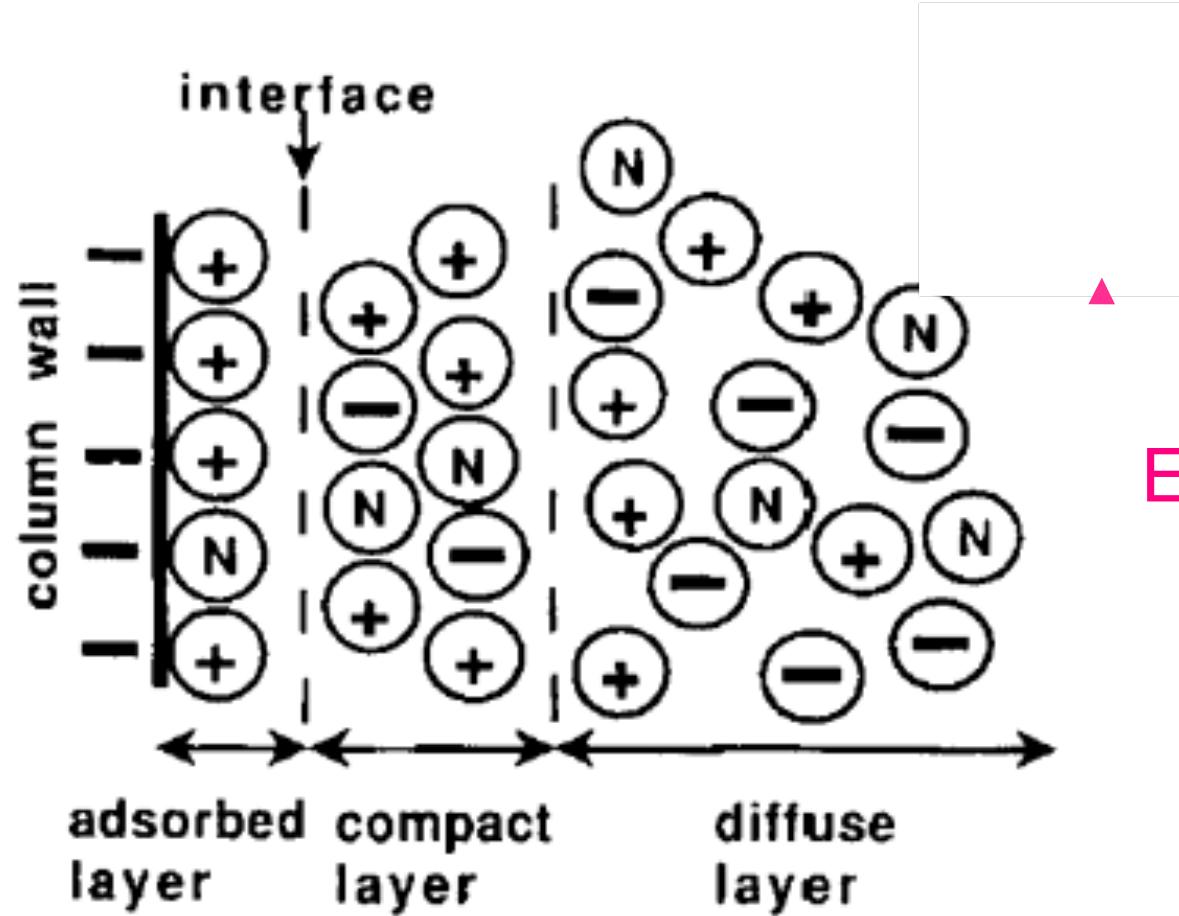
Integrated virtual optical machine



PY Chiou, AT Ohta, MC Wu, *Nature* 436, 370-372 (2005)

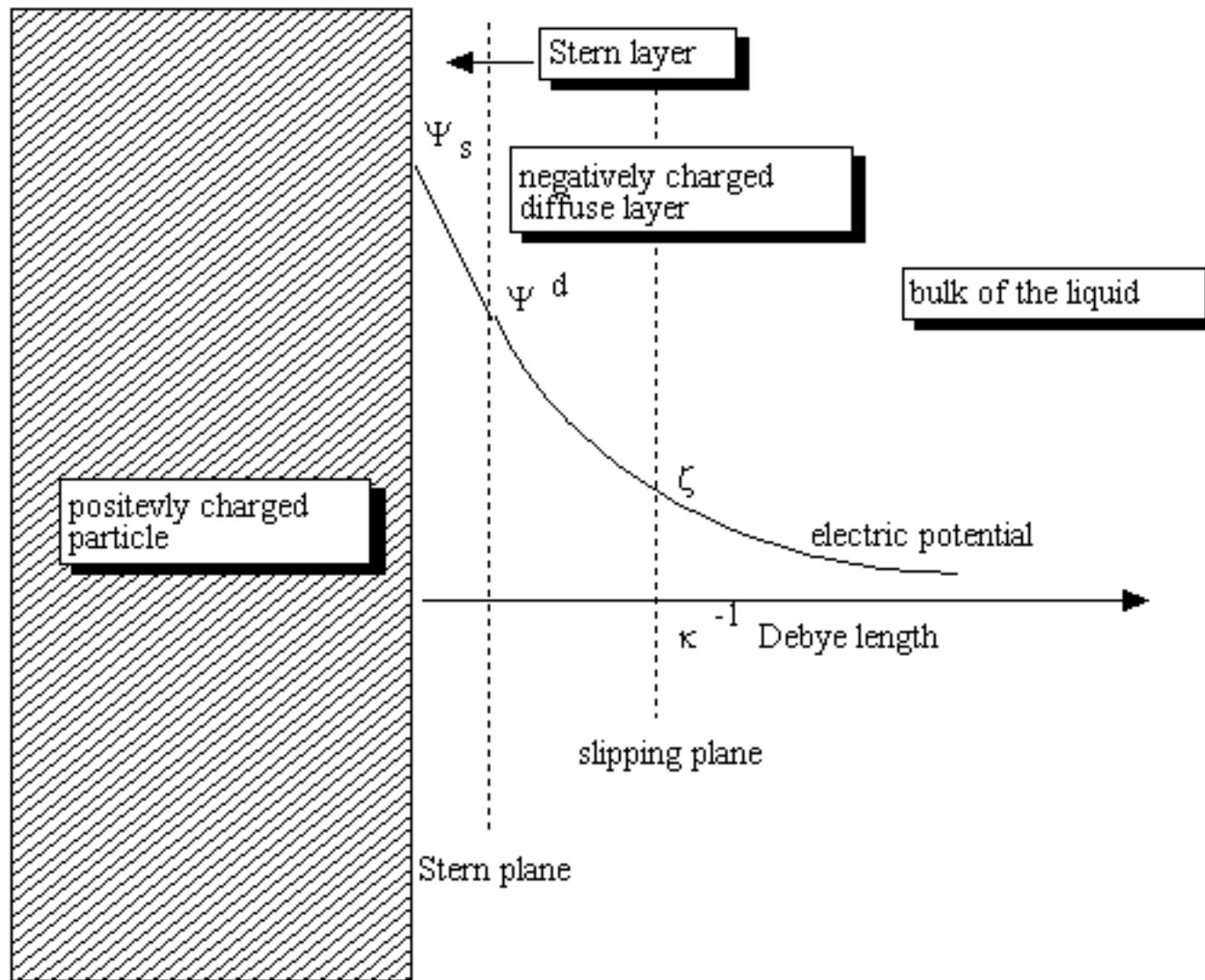


Electrical double layer (Gouy-Chapman-Stern model)





Electrical double layer



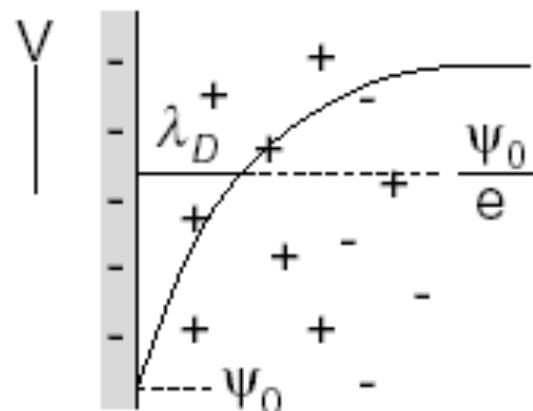


Poisson-Boltzmann Equation

Poisson Eq. $\nabla^2 \phi = -\frac{\rho_E}{\epsilon}$. Boltzmann distribution: $c_i = c_{i,\infty} \exp\left(-\frac{z_i F \phi}{RT}\right)$.

Poisson-Boltzmann Eq.

$$\nabla^2 \phi = -\frac{F}{\epsilon} \sum_i c_{i,\infty} z_i \exp\left(-\frac{z_i F \phi}{RT}\right).$$



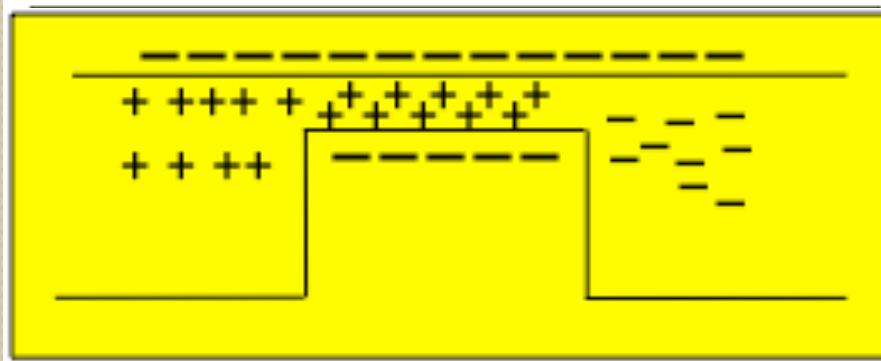
$$\lambda_D = \sqrt{\frac{\epsilon R T}{2 F^2 c}}$$

Conc / M	λ_D / nm
10^{-5}	100
10^{-4}	30
10^{-3}	10
10^{-2}	3
10^{-1}	1



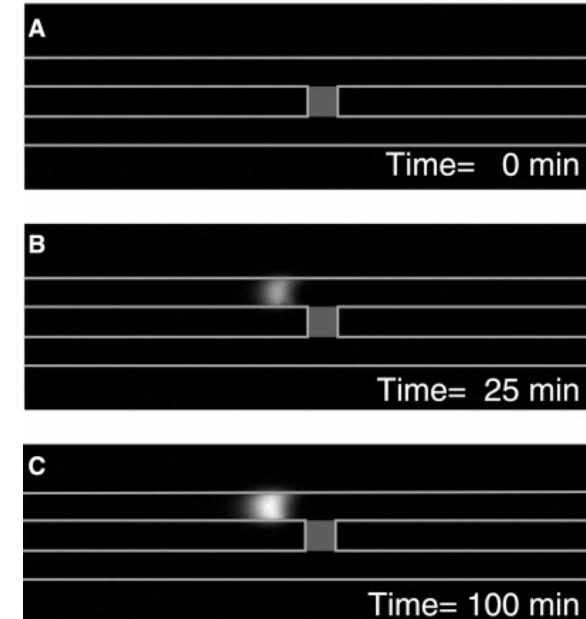
Debye layer overlapping

Field OFF



Nanoconcentrators

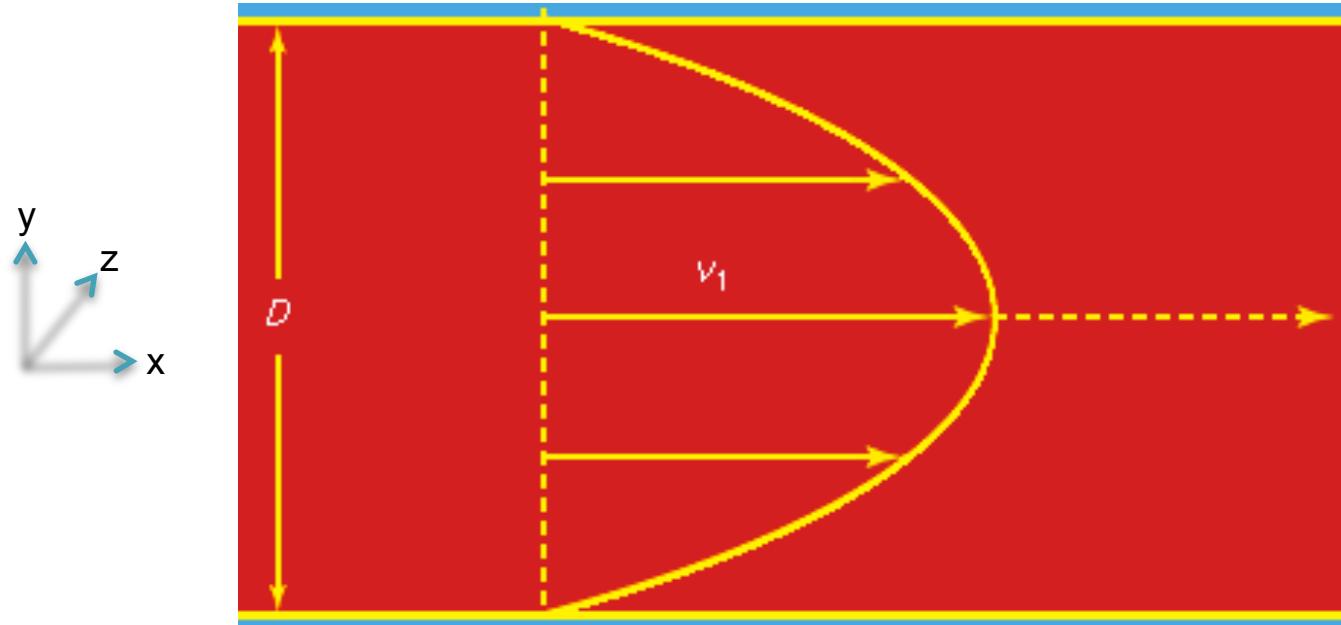
Wang et al., Anal. Chem. 2005





Pressure-driven Poiseuille Flow (parabolic)

$$v_x(y) = \frac{1}{2\eta} \frac{\Delta p}{l_x} [(a/2)^2 - y^2]$$

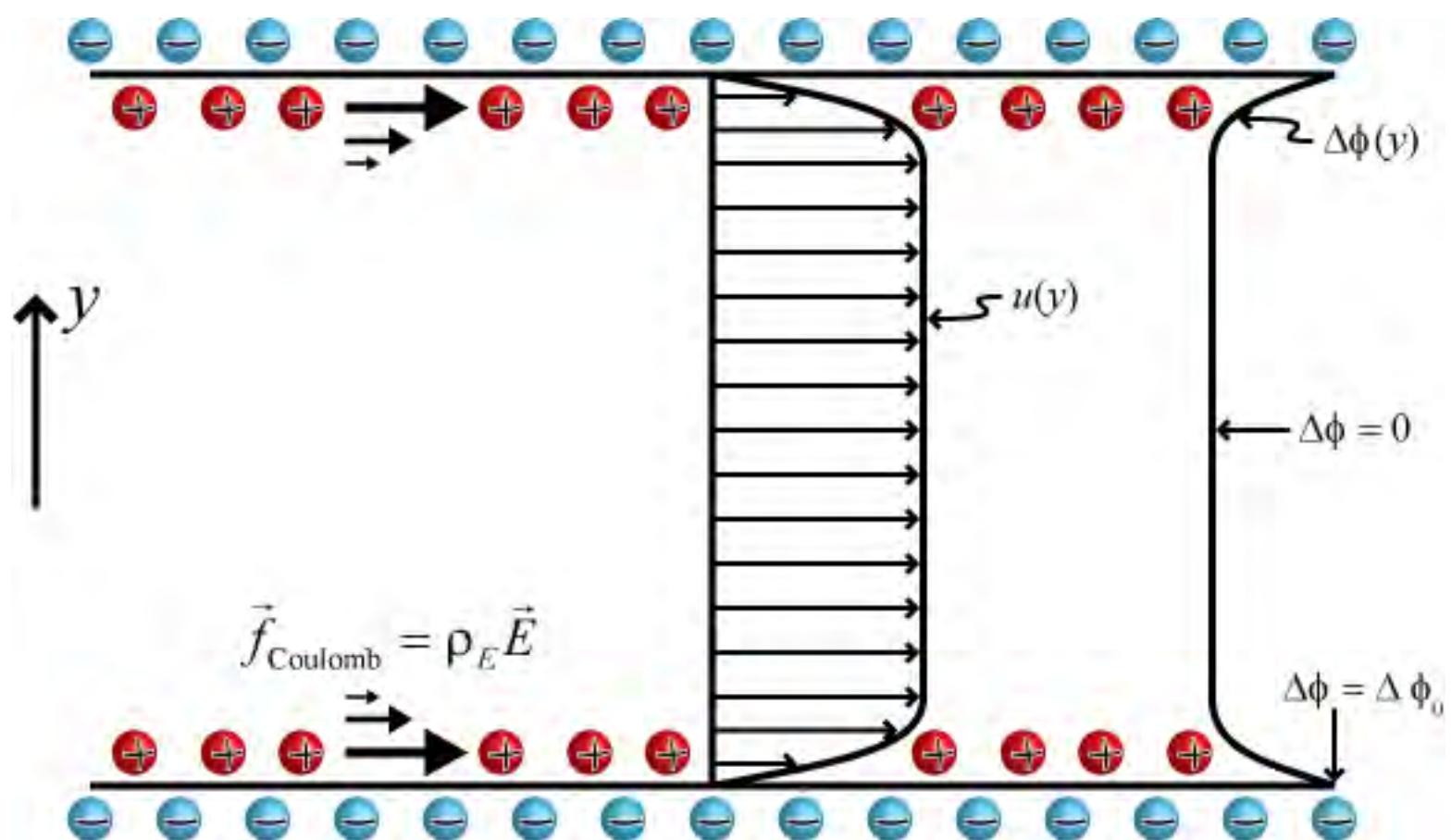


Ref. Lecture Notes on Micro/nanofluidics



Electrical double layer and electroosmotic flow

$$f_{\text{DEP}} = 2\pi r_p^3 \varepsilon_m Re(f_{\text{CM}}) \nabla E^2 \quad \text{"Plug flow"} \quad f_{\text{EK}} = -6\pi\eta r_p \mu_{\text{EK}} E$$





Electroosmosis flow

Electroosmotic mobility: $\vec{v}_{\text{Surface},\text{wall}} = \mu_{EO} \vec{E}_{\text{ext},\text{wall}}$

WALL MATERIAL	SOLUTION	μ_{EO}
glass	pH7, 1 mM NaCl	$3 \times 10^{-8} \text{ m}^2/\text{V s}$
glass	pH5, 1 mM NaCl	$1 \times 10^{-8} \text{ m}^2/\text{V s}$
silicon	pH7, 1 mM NaCl	$3 \times 10^{-8} \text{ m}^2/\text{V s}$
poly(dimethylsiloxane)	pH7, 1 mM NaCl	$1.5 \times 10^{-8} \text{ m}^2/\text{V s}$
polycarbonate	pH7, 1 mM NaCl	$2 \times 10^{-8} \text{ m}^2/\text{V s}$

$$\mu_{EO} = -\frac{\epsilon \varphi_o}{\eta}$$

Electrokinetic potential or zeta potential: $\zeta = -\frac{\mu_{EO} \eta_{bulk}}{\epsilon_{bulk}}$

ζ is an experimentally observed quantity that has units of volts. If the fluid has uniform ϵ and η , then the measured ζ is equal to ϕ_o . If the fluid permittivity or viscosity vary in the electrical double layer, then a different integral analysis must be performed to relate ζ to ϕ_o .



Steering of particles by Electroosmotic Actuation



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Exercise (due 1/5/2011)

- E. coli coasting time and distance? Assume radius is 1 micrometer, velocity 30 um / s.
- Diffusion (random walk) which is not Gaussian? Give an example. (Steve Granick).
- Describe an experimental technique which is capable of measuring zeta potential.